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SYSTEM AND PROCESS DEVELOPMENT FOR SELECTION OF HIGH STRESS TOLERANCE PERSONNEL

by Albert F. Ax

Prepared by
LAFAYETTE CLINIC
Detroit, Mich.

for Ames Research Center

NATIONAL AERONAUTICS AND SPACE ADMINISTRATION • WASHINGTON, D. C. • SEPTEMBER 1968



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Prepared under Contract No. NAS 2-1031 by LAFAYETTE CLINIC Detroit Mich.

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ABSTRACT

A system has been developed for digital computer processing of psychophysiological data. It employs oscilloscope and oscillograph display, analog magnetic tape storage, A/D conversion, digital tape storage and a large digital computer (IBM 7094). The computing programs developed select all points of interest and compute their type, time of occurence, amplitude and curvature. A summary program computes the mean and standard deviation for the response parameters of amplitude, slope, curvature, duration and interval for any set of epochs selected by the editor. A third program selects pairs of points from any sets of variables on the basis of minimizing the variance in lag for the set. The coincidence coefficient and product moment correlations are computed for any set of response parameters of paired points chosen by the editor. These correlations do not confound coincidence, amplitude and shape of responses as does the classical cross-correlation function and are therefore more suitable for the study of the interdependence of biological subsystems.

Two substantive studies have been completed. The classical conditioning of autonomic responses in schizophrenia and healthy subjects demonstrated a marked impairment in the performance of autonomic conditioning by schizophrenic patients. A pilot study of non-schizophrenic low motivation subjects revealed a disability for autonomic conditioning similar to that found in chronic schizophrenia. These findings suggest that autonomic conditioning may serve as an index for the diagnosis of both schizophrenia and low motivation and permit the speculation that a low aptitude for autonomic learning may be a contributing factor to both schizophrenia and low social motivation. Finally a study of physiological concomitants of psychological differentiation suggests that the

degree of autonomic response differentiation may be correlated with the cognitive style of perceptual discrimination.

It was concluded that these successful demonstrations of the diagnostic power of psychophysiological data and those of digital computer analysis justify further study and development of this approach.

These studies are of value to NASA and the science of human motivation and emotional development by virtue of progressing toward more accurate selection and rapid training of personnel for high stress tasks.

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I. Purposes of the Study.

The primary purposes of this study were to develop a system for processing psychophysiological data and to apply it to the task of developing indices for the diagnosis of human tolerance for stress. It was recognized that aptitudes for learning motives and emotional control were primary components of stress tolerance. In order to contain the scope of the investigation within practicable limits imposed by our resources only the psychophysiological aspects of motivation and learning were considered.

The context of the study has two salient features. The psychophysiology laboratory at The Lafayette Clinic had just completed the development of a processing system for psychophysiological data utilizing and EPSCO data logger consisting of a 29 channel multiplexor and a 10 Kc A/D converter and a Bendix G15-D computer with special programs developed for the purpose. That study demonstrated the approach to be feasible but relatively impracticable because of the limitations in capacity and speed of the computer. The other favorable aspect of the situation was that the state-of-the-art of the psychophysiological methodology was just approaching the level to justify major effort toward massive data processing. Biomedical monitoring was being used with pilots, astronauts and in hospitals. Active research was under way in several score laboratories supported by federal agencies, private industry and at medical schools and hospitals. The Society for Psychophysiological Research had been organized two years previously (1960) and the journal PSYCHOPHYSIOLOGY was being established. Psychophysiology thus appeared to be mature enough for marriage to a high speed data processing system.

Psychophysiology is one of the approaches which seeks to explain the physiology of behavior. It focuses on covert behavior available for measurement at the skin surface. It utilizes electrodes and sensitive transducers to sense physiological processes in target organs of the autonomic and central nervous systems and of the endocrine systems. Its special advantages are: (1) that its methods can obtain quantitative, continuous measurements of vital processes whose changes are often too small or fleeting to observe clinically: (2) the measurements can be made without seriously disturbing the processes being observed by intrusions such as implanted electrodes; and (3) the data obtained are already organized in terms of the target organs.

Psychophysiology has its special problems to overcome. (1) Each target organ response may be an end product of several influences, hence may not be a pure measure of any one. (2) This complexity of determination requires the simultaneous measurement of several variables so as to "triangulate" on the processes of interest. (3) The multiple variable approach necessitates complex recording and data processing equipment.

The study of intact systems without subsystem isolation (often referred to as "closed loop analysis") is sometimes criticized as unproductive for the study of the human organism because the system is so large and complex, the transfer functions so poorly described and the number of available variables so small relative to the complexity of the system that the correct interpretation of findings may be impossible. In a sense the description and prediction of human behavior is like describing and predicting the weather—both are large, complex, open, dynamic systems requiring multiple variable, closed loop analysis. More accurate prediction for both require more variables, more observation points and more sophisticated data processing than has so far been possible.

During the past 20 years large scale computers have been applied to weather prediction enabling marked advances in accuracy. We believe similar progress can be made for limited areas of human behavior such as stress tolerance, motivation and emotional control.

The analogy between weather and behavior should not be pushed too far.

There are many obvious differences. One important difference is that weather is determined largely by energy transfer whereas behavior is controlled chiefly by the transfer of information. Hence the principles of information theory rather than energy transfer functions are more appropriate for the study of behavior of living organisms. Signal recognition and signal production with multiple level feedback interactions are characteristic of living organisms. For this reason the experimental design and the data processing must be appropriate to signal manipulation which involve sensory thresholds, adaptation or learning, reinforcement or motivation, differentiation and generalization.

We have discussed this psychophysiological position in more detail elsewhere (Ax, 1964). An appreciation of this viewpoint is helpful for the reader to understand certain features of the experimental design, the data processing, hardware and the computer programs, as well as our interpretation of the results.

One limitation which psychophysiology shares with all science (except possibly astronomy) is the "general principle of uncertainty" used in the sense that our observations influence the phenomena under observation. The attempt to measure simultaneously as many variables as possible, to control the local environment and to standardize all procedures and instructions to subjects, etc. may influence the subject's behavior, especially his natural emotions, to such

an extent that every effort to increase these laudable scientific controls is defeated by a "law of diminishing return". Good psychophysiologic technique strives to minimize the influence of the observation procedures by employing miniature non-painful sensors and by creating a test situation as natural as The use of telemetry to replace the umbilical linkage is one further step that is being taken to enable psychophysiological observation on the free roaming individual while pursuing his natural activities. This next step in psychophysiological methodology adds a severe burden to the data processing. Much more noise is introduced due to movement artifacts and uncontrolled environmental influences as well as the degradation of the signal by the radio linkage. The problems of noise elimination and pattern recognition problems for machine editing has been discussed previously (Ax, Andreski, Courter, DiGiovanni, Herman, Lucas, and Orrick, 1964) and later in this report. Recording may be carried out over days or weeks which strains both the sensor reliability and the capacity of the data processing system. Sampling rates and programming must be carefully planned to minimize the computing time and cost while at the same time maximizing information obtained. Only just sufficient redundancy of sampling to achieve reliability can be tolerated.

One final general aspect of the psychophysiological approach should be mentioned before plunging into the details of the study. Psychophysiology has certain characteristics, advantages and disadvantages as compared to the classical physiological methods. The chief advantage is its ability to obtain information about physiological system status and process without damage or discomfort to the organism. A second advantage is the organization of the response system provided by the end organs. The vasoconstriction response at a finger tip is often much easier to interpret as a functional response relevant

to the organismic intentions than is the neuronal response train from an electrode implanted deep in the brain. Similarly, the current activities of the brain may more readily and understandably be described by a pattern of end organ responses such as arterial tonus, muscle tonus, heart rate, heart stroke force, blood pressures and palmar sweating than it can from the EEGs from 32 electrodes scattered about on the scalp. The "face validity" of the EEG as a prime psychophysiological measure for brain activity has often been overvalued due to its success in helping to locate a gross physical damage of the brain. Actually the neurological examination (a clinical type of psychophysiological examination) is often more definitive for brain malfunction. Many psychophysiological variables other than EEG are excellent indices of arousal or motivational state. EEG is one useful physiological measure but has little special value simply because its sensors are located physically closest to brain tissue. A. T.V. repairman does not diagnose a malfunction by scanning the electric field strength over the cabinet of the T.V.; rather he measures potentials and currents in logically critical circuit points. The sensor and effector organs of the body are logical points for the organism. No criticism is implied of the excellent studies of brain structure and functions by direct examination of brain tissue by neurophysiologial methods. It is emphasized that total organismic processes such as emotion, motivation and "stress tolerance" are much more likely to be monitorable by patterns of end organ responses than by scalp EEG.

II. METHODS

A. Data Acquisition System.

Research employing continuous recording of multiple variables requires high speed computing for two reasons: (1) to transcribe the necessarily large numbers of samples into digital values and (2) to compute the multiple interactions among the variables involved. The transcription aspect for a single one hour session for only 10 physiological variables (not including EEG) may require as many as 36,000 samples to describe the variables. An average study of 5 sessions per subject and 100 subjects would produce 18,000,000 values; and many studies might require more variables, more recording per subject, or faster changing variables (such as EEG) which would greatly increase the amount of data to be transcribed and summarized. The computing aspect merely for means, variances, t-tests, and correlations among the parameters that can be abstracted from a set of 10 physiological variables is quite a large task without the aid of a digital computer. When more sophisticated statistics such as factor analysis and multiple regression are employed the computing multiplies many fold. Any method of processing such data less powerful than the digital computer is impracticable for large scale studies required for exploitation of the psychosychophysiologic approach.

A brief preview of some of the problems encountered in developing a high speed system for processing psychophysiologic data may be of interest. Analog computing was considered and rejected as impracticable because an analog computer sufficiently large to handle all variables simultaneously in real time would be too costly. Analysis of single variables or pairs for correlation

from magnetic tape storage by a medium-sized analog computer would probably be practicable but still probably slower and require a more costly installation although this approach might have been competitive to the digital system. A further reason for going digital is that automatic computing by the stored program digital computer is very efficient and flexible.

Once the specific digital computer to be used had been identified (for us an IBM 7094), then all design characteristics had to be made compatible with it. The digital tape recorder must meet 7094 specs; the AD converter must produce the specified format, packing density, parity bit, and other specifications. The ADC must have sufficient resolution which for us was 12 bits (1 part in 4096) to cover any range expected. For example if the palmar skin resistance has a range from 30,000 to 1,000,000 ohms and if a GSR as small as 200 ohms change is to be resolved the full dynamic range of 12 bits is needed. The multiplexor must be able to sample at a rate sufficient to sample all variables sufficiently fast to resolve the most rapid changes to be encountered. We judged that 10 samples per minimum expected period would be adequate. For a selection of 30 variables of varying rates of change we chose 160 samples per second real time for all 30 variables (10 at 10 per second, 10 at 5 per second and 10 at 1 per second). A multiplexor with 30 inputs was chosen with an eye to expansion but experience has shown that other difficulties and limitations make it unlikely that more than 10 to 15 variables can be handled, unless groups of subjects are studied simultaneously.

On-line analog preprocessing of most variables in various degrees is required. Nearly all variables require some filtering. Some variables like EKG for our purposes of obtaining heart rate require a cardiotachometer to detect the time of the QRS complex and convert the time between adjacent

QRS complexes into a voltage to be presented to the ADC. The step change, square wave aspect of cardiotachometer data makes it difficult to use. Most sample-and-hold circuits drift slightly and in opposite directions depending on whether the value is above or below zero potential; thus the high or low point to be picked by the computer might be either at the beginning or end of the heart cycle and thus make ambiguous the time of the point. The solution to this problem appears to be to produce a pulse at the time of the QRS whose amplitude represents the duration of the last HP and whose duration is greater than one ADC sample period but less than two, thus assuring a sample as early as possible after the information is available but none at any other time. Between readings the cardiotachometer would assume a value off scale enabling the computer to readily ignore those valueless samples.

Other problems that must be handled for automatic data processing involve solutions to the noise or artifact problem and precise calibration through the entire system from transducer to computer. Filtering and human editing (described in detail in the software section) take care of the artifact problem. Automatic editing seen as a problem of computer pattern recognition is considered a research and development problem. Practicable total system calibration requires excellent stability of component systems both as to gain and base line. A practicable system must be able to be quickly checked and adjusted by the operator and not require an engineer. Finally short term instability should be self checking possibly by supplying frequent calibration signals to the computer which could then modify the output conversion values so as to make them correct.

1. Overview.

The block diagram of Figure 1 shows the plan of the system.

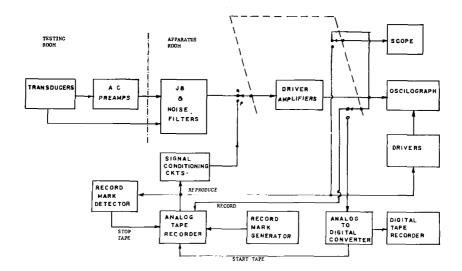


Figure 1

The sensors on the subject and the preamplifiers are in the observation room. The rest of the apparatus is in the adjacent instrument room. During a recording session, the amplified signals are displayed on an 8-channel oscilloscope and recorded on a 24-channel oscillograph and on a 14-channel FM magnetic tape recorder. For computer analysis at a later time, the signals are reproduced from the tape recorder, modified by signal conditioning circuitry, rerecorded on the oscillograph, sampled and digitized by the 29-channel analog-to-digital converter (ADC) and recorded on a digital magnetic tape in IBM 7094 format.

2. Observation Situation.

The subject room is 12x14x8 feet, accoustically insulated and

temperature controlled to 25.5 ± 0.2 C. Humidity is uncontrolled but is recorded as are the outside environmental conditions of temperature, humidity, and barometric pressure. Two one-way observation ports and complete intercom with audio magnetic tape recording are provided. The subject enters directly from a corridor (not through apparatus room) and reclines on the ballistocardiograph bed. Sensors are applied and plugged into jack panels on either side at the head of the bed. Preamplifiers are near the subject for EMG, EEG, EKG, finger pulse and body movement.

3. Sensors.

(a) Electrodes.

Variables sensed by electrodes are the electrocardiogram (EKG), electroencephalogram (EEG), electromyogram (EMG), impedance plethys-mogram (IPG), skin potential (SP), and skin conductance (SC). Other electrodes are used for grounding the subject and for applying electrical stimulation.

(b) Transducers.

These are used for sensing skin temperatures (ST), chest and abdominal circumference to measure respiration (CR & AR), the ballisto-cardiogram (BCG), finger pulse (FP), body movements (BM), and blood pressures (SBP, DBP).

4. Display and Recording.

All signals, except muscle potentials, after preamplification associated with their transducers are filtered and amplified by Offner type 492 DC amplifiers. The signal is then split into three: one branch goes to the 17", 8-channel oscilloscope and is recorded on an oscillograph (24-channel, model 1108 Honeywell) and the third branch goes to the analog magnetic tape recorder (Ampex model CP 100, 14-channel FM). Several signals may be multipexed on the oscilloscope and tape recorder so as to accommodate them all.

During the recording phase, a 1-per-second timing pulse (of 300 CPS for a period of 50 MS) is recorded on the face temperature channel. An electronic counter causes every tenth signal to actuate a marker channel of the oscillograph.

5. Identification Mark for Analog Tape.

Since several experimental sessions may be recorded on one roll of magnetic tape, a system is required for marking and locating the beginning of specified records. This record start mark is recorded on the tape and also displayed on the oscillograph chart, so that precise synchronization can be achieved between the record made during recording and the one made during reproduce which is used for editing. The record mark is a decimal number coded in binary by two voltage levels on each of the 14 channels of the analog tape. Its maximum value is 3999. Each recording session is given a sequential identification number (ID). A particular record may be located on a reel of analog magnetic tape by setting the decimal controls at the desired ID number. The ID numbers are displayed on Nixie tubes as they are passed and the tape stops on the preset ID number. By adding an additional unit any point within a record could be located to the nearest second. have not found any need for this feature, hence, it has not been added, in line with our general philosophy of keeping the apparatus as simple as possible consistent with required performance.

B. Data Processing System.

1. Signal Conditioning.

Since the ADC sampling switch requires either a synchronized signal or the continuous presence of the signal, the discontinuous asynchronous pulse variables such as EKG, plethysmogram and BCG require transformation before conversion. The EKG is used to generate the heart period (HP), the peripheral

pulse amplitude of the finger plethysmogram (FP) is detected by a peak reading hold circuit, and for BCG the IJ wave is measured and held until the next EKG opens the gate for the next BCG signal. The EMG and body movements are integrated, sampled and held. EEG may be analyzed directly in the high-speed mode or it may be divided into several frequency bands and each band displayed as a continuous voltage equivalent to the smoothed average power or voltage of the signal within the band. Any period of EEG record can be analyzed in the high-speed mode of the regular "Points of Interest" program described in the section on software. Since, however, this type of micro-analysis can be quite costly, the more economical, though less detailed method of abstracting the average voltage or power from several broad bands is more practicable.

The DC or slowly changing variables such as temperatures, respiration, palmar conductance and skin potential are reproduced from the analog tape and sent to the ADC essentially unchanged except for amplification and filtering.

The signal conditioning circuitry is the stage where automatic editing for artifacts will be done. At present only filtering, gating by EKG for BCG and PP and the simple pattern recognition of the IJ portion of the BCG are used. More sophisticated pattern recognition circuits are being designed to better distinguish between clean signals and artifacts. Most artifacts caused by subject movements are now removed by the human editor as described in b, (4) of the software section.

2. Digital Magnetic Tape Formats and Sampling Rates.

Economy in digital computation requires the minimum sampling rates consistent with the type of information desired for each variable.

It was decided that a sampling rate of 10 samples per minimum interval of variable would provide sufficiently detailed information for our purposes.

Thus if maximum respiration rate were 1 per second, 10 samples per second would enable sufficiently accurate location and amplitude determinations required for computing respiration period and an index of tidal volume. Similary the heart period can change from a maximum of about 2.0 seconds to a minimum of about .33 seconds (30 to 180 beats per minute) in not less than 1/3 second. A sampling rate of 3 SPS would suffice; but because of our desire to correlate the coincidence of changes as well as amplitude changes of heart and respiration periodicity, it was decided to sample the cardiac variables also at 10 SPS so as to make the time of corresponding points on correlated variables equally precise. The slow-changing variables like temperature and those integrated for a definite time of 1 second are sampled 1 SPS. A sampling rate of 5 SPS was chosen for skin potential. order to provide for the future addition of variables, the ADC sampling switch was designed to provide 10 variables at 10 SPS, 10 at 5 SPS and 10 at 1 SPS including a nonsampled time code generated at 1 SPS. Together these total 160 SPS in real time or 1280 SPS in the reproduce mode as actually used (8:1 speedup). Because of the inherent high-speed sampling and conversion capability of the solid state converter, and an expectation that higher frequency variables such as EEG might sometime be analyzed, a high-speed mode of 6400 SPS is also available. Thus for the high-speed mode there are 10 channels each at 400 SPS, 10 at 200 SPS and 10 at 40 SPS. When this mode is used, the analog record and playback is 1:1 and the digital tape operates at 25"/sec producing the same bit density of 512/inch used for the low-speed mode in which the tape speed is 5"/sec.

a. Density and Sampling Rate.

The raw data is recorded on a digital tape for input

to a 7094. The tape is recorded at 512 bits/inch in binary (odd parity) mode. The data is recorded in long physical records with the data samples packed and interlaced. The present system accommodates 30 channels of data sampled at 3 different frequencies.

Channels 1 - 10 Sampled 10 times/second.

Channels 11 - 20 Sampled 5 times/second.

Channels 21 - 30 Sampled 1 time/second.

Channel 30 contains a time code generated by an internal clock in the ADC rather than data.

b. Tape Layout.

Each physical reel consists of 1 or more recording sessions of up to 1.14 hours each. Each session is preceded by a short identification record. The ID record consists of a 12-octal digit ID number repeated 8 times. This ID number is generated by a set of 12 octal switches on the ADC which are manually set.

The 8-word ID record is followed by one or more data records. Each data record consists of 6720 36-bit words representing 126 seconds of real time data. Following the data record is a 1 1/4" interrecord gap. The gap is generated by stopping the ADC without stopping the tape and represents a loss of 2 seconds worth of data out of each 128 seconds of real time.

The last physical record in the session is followed by an end of file mark. The last end of file mark on the reel is followed by an ID block with an ID number of all sevens, (77777777777).

c. Data Sample Packing and Interlace.

Each data sample consists of 12 bits, 11 bits plus a sign bit, thus each sample is a number limited 2048 > sample > -2048. Samples are packed 3 per computer word. Sampling of data channels proceeds in "frames"

of 1 second each, the pattern being repeated once per second. A tape record is 126 frames or 6720 words long. Each frame is sampled as follows:

1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	
_	_	_	-	_	-	-	-	_								
1	4	3	4	2	O	/	Ö	9	ΤO	Τ/	TQ	19	20	21	22	
1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	
1	2	3	4	5	6	7	8	9	10	17	18	19	20	23	24	
1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	
1	2	3	4	5	6	7	8	9	10	17	18	19	20	25	26	
1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	
1	2	3	4	5	6	7	8	9	10	17	18	19	20	27	28	
1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	
1	2	3	4	5	6	7	8	9	10	17	18	19	20	29	30	

Sampling procedes from left to right. When read into the computer starting in location 1 the following pattern results:

Word	S-11	Samples in Bi	t Positions 24-35
00001	1	2	3
00001	4	5	5 6
00002	7	8	9
00004	10	11	12
00005	13	14	15
00006	16	1	2
00007	3	4	5

etc.

4. Time Codes.

The time codes generated by the A/D converter and written on the tape as data samples for channel 30 are slightly different from ordinary samples in that they are unsigned 12-bit intergers. The clock counts in 1-second intervals from 0 to 4095 and counts modulo 4096.

The first time code on the tape in a session is 3, the last time code in the first physical record is 128. The interrecord gap represents two seconds, i.e., 129 & 130, thus the first time code in the second physical record will be 131.

5. Variations From Standard IBM Tape Format.

Tapes produced by the ADC while entirely compatible with IBM

729 Model IV or 729 Model VI tape drives have, none the less, certain variations from standard IBM formats.

- (a) Density Tapes are recorded at 512 rather than 556 bits/inch.
- (b) Interrecord gaps Interrecord gaps between data records are 1 1/4" rather than 3/4". The gap after the 8-word ID block is approximately 79". (The ADC produces only 6720 word records. Even though the ID block is only 8 words long, it writes enough blank tape to make a 6720word record).

3. Software.

a. Overview.

This section deals with the computer programs*. The programs as described are operational at the General Motors Technical Center computing laboratory. Since, however, their monitor system is unique, the programs as now written cannot be run directly on other 7094 installations. Mr. Singer and Mr. Stahlke in collaboration with the personnel at the NASA Ames Computing Center modified the programs so they can be run at NASA Ames Research Center. To run the programs at other computing centers would usually involve still other modifications as required by each local installation. If the programs were to be applied to different data tape formats, modification of the input routines would be required. The cards and listings for the operational programs may be obtained from The Lafayette Clinic, attention A. F. Ax.

The programs were designed to automate the analysis of physiological

^{*} Programming was done chiefly by Samuel Singer with the help of Rudy Stahlke, Barbara Levin, Robert Hirschfeld, and James Licholat.

data by the use of a high-speed digital computer. A very large amount of data can be accumulated in a very short time in biological experiments in which many variables are studied simultaneously. The data acquisition system for which these programs were designed produces about a half million data samples per hour. Clearly this amount of data must be reduced to something more manageable by extracting only the most significant information, and perhaps equally important, it must be done at a reasonable cost.

With a problem of this magnitude it is important that the system as a whole be fast and efficient, yet it must be flexible to the greatest degree so that a variety of problems can be solved. Data storage was designed with minimum storage space and maximum speed of data retrieval in mind. Where compromises between speed and complexity were necessary, they were generally made on the side of greater speed.

The sections that follow describe the programs in some detail and also the logic involved in the choice of these particular solutions.

- b. Points of Interest Program.
 - (1) The Response Concept.

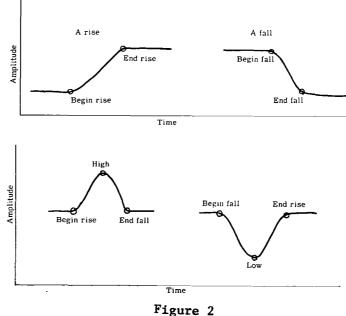
The data analysis is based on the concept of <u>biologic</u> response (Ax, 1958; Ax, Singer and Zacharopoulos, 1962; Ax, Singer, Zachary, Gudobba, and Gottlieb, 1964), which may be defined for any variable as a significant change in amplitude within a specified time limit. The question which must next be answered is, what is a "significant" change? Since there is a certain amount of "noise" inherent in any system, the amplitude of change must at least exceed the noise level and since there is a certain amount of homeostatic drift in amplitude with time, we may

realistically say the significant change in amplitude must occur within a certain time limit. The response is therefore defined in terms of two tolerances, an amplitude tolerance and a time or duration tolerance. A slope could not be used for the tolerance since noise may have high slopes. A response is an amplitude change that occurs within a duration tolerance and exceeds an amplitude tolerance.

A response may be either an increase in amplitude, a rise, or a decrease in amplitude, a fall . It begins when the variable changes amplitude by more than an amplitude tolerance within the period of one duration tolerance and ends when the variable no longer changes amplitude by more than an amplitude tolerance within the period of one duration tolerance. Since one response may immediately follow another, we must also say that a response ends when it changes direction.

(2) Points of Interest.

Responses are identified by their end points which are called Points of Interest (PI). The points are named according to the response they delimit. Examples (Figure 2) are Begin Rise (BR),



End Rise (ER), Begin Fall (BF) and End Fall (EF). The figures illustrate examples and Table 1 lists all points and their abbreviations.

Types of Points	Abbr.	Comment
Begin Rise	BR	CURV Computed
End Rise	ER	CURV Computed
Begin Fall	BF	CURV Computed
End Fall	EF	CURV Computed
High	ні	CURV Computed
Lou	LO	CURV Computed
Drift High	DH	No CURV Computed
Drift Low	DL	No CURV Computed
Begin Epoch	BEP	No CURV Computed
End Epoch	EEP	No CURV Computed
Begin Edit	BE	No CURV Computed
End Edic	EE	No CURV Computed
Begin Short Edit	BSE	No CURV Computed
End Short Edit	ESE	No CURV Computed

Table 1

For the case in which one response does not immediately follow another, the portion of curve between two responses is known as a <u>drift</u>; and if the drift is of less than two time tolerances in duration, it is called a plateau. Examples of these cases are shown in Figure 3.

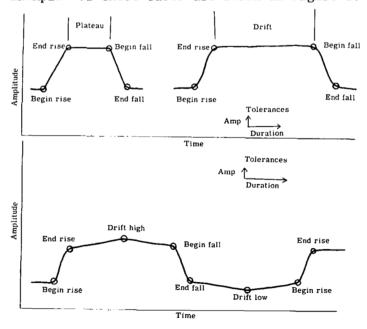


Figure 3

A drift may be of any duration. If during a drift the amplitude exceeds both end points by an amplitude tolerance, the extreme is identified as a <u>Drift High</u> (DH) or <u>Drift Low</u> (DL). A cumulative response consists of two or more discrete responses separated by plateaus (see Figure 4), but not by drifts.

The amplitude of a cumulative response is measured from the first begin rise to the last end rise.

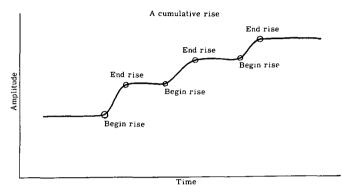


Figure 4 Data are

generally recorded within a certain experimental design. The recording period is divided into one or more experimental epochs. It is usually desirable to identify the limits of an experimental epoch. This is done with special points of interest called Epoch Points (EP). These may or may not coincide with one or the other points of interest.

The points of interest are written on magnetic tape ordered by variable number in ascending time sequence. Each P.I. consists of (1) variable number, (2) amplitude, (3) time, (4) type (Hi, Lo, ER, etc.) and (5) curvature. These 5 values for each P.I. are packed into two words on the P.I. tape.

(3) Curvature.

.We have now arrived at a set of parameters called Points of Interest which describe a curve. They have the virtue of being easy to obtain rapidly and of describing many important features of

the data concisely. One disadvantage of the Points of Interest is that they describe responses (our primary interest) only at their ends and say nothing about what happens between. Further information can be obtained as is illustrated by the cases shown in Figure 5.

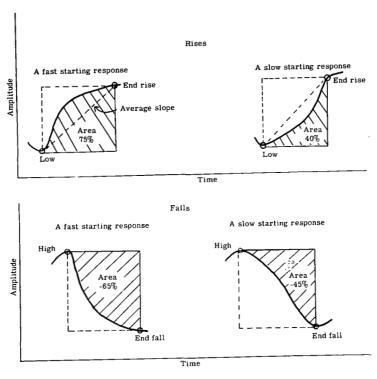


Figure 5

The first two responses shown have similar end points but different behavior in between. In one sense we might call the first a big response or fast-starting response and the second a small or slow-starting response. The area under the response, shown cross-hatched, is a good index of the difference between the two responses. A fast-starting response has a large area. The area is a way to describe the average curvature. Areas larger than the triangle enclosed by the average slope line indi-

cate a generally convex curve produced by a "negative acceleration" over most of the curve. Conversely areas less than the triangular area indicate a generally concave curve. To preserve this property of a fast-starting response being associated with a large area the complimentary area, or area over the curve, is computed for falling responses. In order to give the area or curvature concept a standard meaning regardless of amplitude, duration or area of the particular response, the percent of the rectangle encompassed by the amplitude and duration of the response is computed as illustrated.

(4) Artifacts and Editing.

Unfortunately real data generally contain a number of artifacts (noise) which must be handled in the data analysis. Indeed, to be generally useful the analysis system should be able to process data that are mostly artifactual and extract what good data are present.

Artifacts may be divided into two groups, those which can be recognized and interpolated or skipped by the computer and those which must be deleted by a human editor. In this system the computer recognizes as artifact those data which exceed either a specified amplitude or a specified slope. These two artifact tolerances are provided by the editor and provision is specified by a third editing tolerance, the edit duration tolerance. An edit of duration less than the edit duration tolerance is linearly interpolated. An interpolated edit is called a Short Edit (SE) while a longer non-interpolated edit is called simply an Edit (E). Their end points are special points of interest and are named Begin Edit (BE), End Edit (EE), Begin Short Edit (BSE), End Short Edit (ESE), as is appropriate. Examples of editing are

shown in Figure 6.

We have now briefly described the essential features of the first part of our data analysis system, the part called the Points of Interest Program (Figure 7). This program which comprises the major part of the system can process several experimental recording sessions sequentially. It can handle 29 different channels of data simultaneously at 3 different sampling frequencies. It has provisions for scaling and converting data to physiological units as well as the features already described. Running time on the IBM 7094 for processing an hour's worth of data (about 500,000 samples for 29 variables) is about five minutes. A sample of

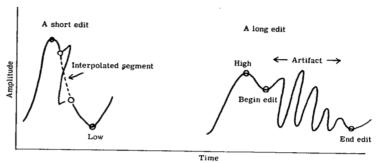


Figure 6

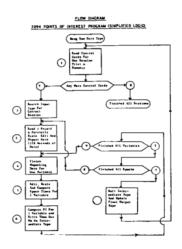


Figure 7

the polygram (Figure 8).

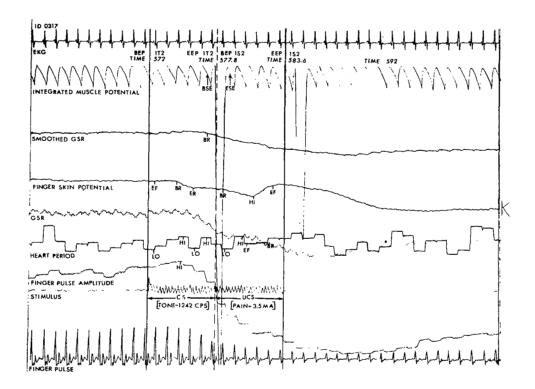


Figure 8

The raw data for all variables (Table 2, appendix) and Points of Interest and summary listing for the sampling of the variables are shown in Tables 3 to 12, appendix..

c. Summary Program.

The Points of Interest Program describes the data in terms of responses. While this considerably reduces the amount of data, the information is not yet organized into a form that is easily assimilated. The summary program is designed to perform the part of this function that does not require elaborate statistical analysis.

The summary program summarizes data by the experimental epochs which

were set up in the design of the experiment. It allows easy comparison of one epoch with another by summating the data. The summary tabulates separately three general categories of data: (1) general information about the epoch, (2) information about the first few responses in the epoch, and (3) a summary of various aspects of all responses for the entire epoch (Table 12a).

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		HEU WAL	754.69	AT TIVE	507.7					
		END AMP	1761.65	AT TIME	9.408					
		MVX VAD	1140.09	AT TIME	894.0					
		ALM WAL	471.79	م بامد	671.1					
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		INIT AMP	INCREMENT	ניתן די אַעות	St Joh	1061	LATENCY	28FC 001CT		
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RESPONSE 3		1271.42	-125.47	1.6	-65.01	-2.41	9.0	2.2		
RESPENSE 4		478.C?	148.95	2.1	70.03	0.47	17.4	2.0		
RESPONSE 5		1175.98	-216.73	4.1	-52.46	-7.3	14.5	ń.		
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			S PER CUM PISS	YFAM =	^. \ \	li = n.				

Table 12a

Each variable is summarized separately. The Summary categories are discussed in more detail below. (See Tables 4, 6, 8, 10, 12, appendix, for computer listing of the summary output for the data whose P.I. were illustrated.)

Table 12a is an example of a standard summary output, but of different data.

(1) General Information Section.

This tabulation permits identification of the epoch and quick evaluation of the range of variation of the variable. It also gives some idea of the amount of useful information extracted by listing the number of points of interest in the epoch and the amount of editing. The following information is listed:

- (a) Variable Number.
- (b) Data Information Number.
- (c) Number of P.I. in Epoch.
- (d) Epoch Number.
- (e) Epoch Duration.
- (f) Epoch Beginning Time and Amplitude.
- (g) Epoch End Time and Amplitude.
- (h) Maximum Amplitude and its Time.
- (i) Minimum Amplitude and its Time.
- (j) Mean Amplitude and its Standard Deviation.
- (k) Percent Good Data.
- (1) Percent Long Edits.
- (m) Percent Short Edits.

(2) First Responses Section.

Experimental epochs are usually set up to study responses to specific stimuli. The largest and most significant responses often occur immediately following the start of the epoch. In order to be able to examine the first part of the epoch indetail, the first few responses are tabulated individually. Up to 10 responses

may be tabulated for a given epoch as well as the first and last intervals in the epoch. The first interval is the period between the start of the epoch and the beginning of the first response and the last interval is the period between the end of the last response in the epoch and the end of the epoch. For each response and interval the following information is tabulated:

- (a) The initial amplitude.
- (b) The amplitude of increment or decrement.
- (c) The duration.
- (d) The mean slope.
- (e) The curvature index.
- (f) The latency time from start of the epoch.
- (g) The preceding drift time between the end of the

 last response and start of the present one. The

 last item, preceding drift, is included to permit ready identification
 those responses that follow other responses immediately and those
 separated by drifts.
 - (3) Summary of Response Parameters Section. (Table 12a.)

This third section of the summary listing (which was not printed out in the preceding examples) tabulates the means and standard deviations of several aspects of the responses in an epoch. Data are tabulated separately for rises, falls, plateaus and drifts. The program also computes cumulative responses if they are present. Cumulative rises and cumulative falls are tabulated separately as well as the mean and standard deviation of discrete responses,

including those in cumulative responses, for each cumulative response.

For each discrete response, cumulative response, drift or plateau,
the number of each type plus the means and standard deviations for
the following parameters are tabulated: (a) increment or decrement;
(b) duration; (c) slope; (d) curvature: (e) interval between responses.

4. Program Input and Output.

The input to the program consists of the session identification numbers for the sessions to be processed, the variable numbers and the begin and end times for each epoch. The data input is the points of interest magnetic tape produced by the Points of Interest Program. Output is printed with an option of writing most of the printed output on tape for future statistical analysis.

- d. Correlation Program.
 - (1) Unconfounded Parameter Correlation.

A method has been developed for correlation of the primary parameters of selected pairs of responses from a single variable or from pairs of variables. It does not employ the conventional auto- or cross-correlation approaches which utilize arbitrary equal interval samples; but rather this novel approach utilizes the time, amplitude, slope and curvature of the responses matched on the basis of minimal variance in lag.

This approach is not only parsimonious in computing time, because a highly selected and much reduced set of points is used, but also it has theoretical value. Consider these two variables in

Figure 9.

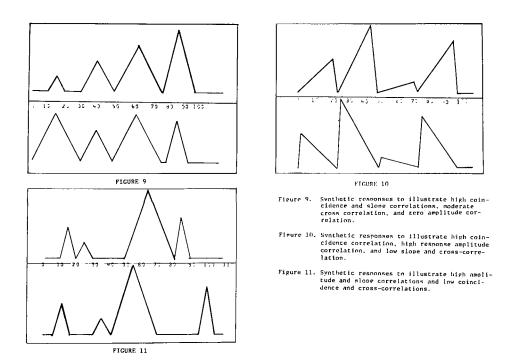


Figure 9

Would you say these two variables are correlated? Note that every time one variable rises to a peak, so does the other, reaching the maximum at exactly the same time. Thus, in the most primitive sense they are perfectly correlated by virtue of their perfect coincidence. We note also that the corresponding responses have exactly similar shapes; in each case the slopes of rise are the same and the slopes of fall identical on the two variables. Thus, their slopes are perfectly correlated. Their maximum amplitudes, however, are completely uncorrelated; the product moment correlation coefficient

of their maximum values is exactly zero. The standard cross-correlation over time applied to these two variables produces a maximum correlation of approximately 0.57 for a lag of zero and less for all other lags. Since a correlation of 0.57 represents about 32 per cent of common variance, we could conclude they are weakly correlated by this classical correlation function; their maximum amplitudes are completely uncorrelated but they are perfectly correlated by indices of coincidence and slope. In the next example (Figure 10) the two variables, when adjusted for lag, have perfect product moment amplitude correlation of their maxima, perfect consistency in lag, but by virtue of their differing shapes produced by differing rise and fall slopes the maximum cross correlation is a minute 0.35 with an optimum time lag of 15.

Finally in Figure 11 the two variables again have responses of perfectly proportionate amplitudes, itendical shapes but this time inconsistent lags.

The maximum cross-correlation whuch occurs at lag 10 is only 0.20.

These examples should make it clear when dealing with variables which have irregular intervals and variable shapes due to different rise and fall slopes, that none of the conventional methods of correlation gives a full and unambiguous measure of their correlation. The standard cross-correlation function based on equal interval samples correlated over a mean time lag (Tau) clearly produces some cort of average, confounded of all three aspects of coincidence, amplitude and slope. In biological systems it may be important to measure any one of these three aspects of correlation independently according to its own internal principles of response. Classical cross-correlation in this situation would reveal only a weak relationship, whereas control may be absolute with regard to occurrence and timing of the dependent systems' response. The neural

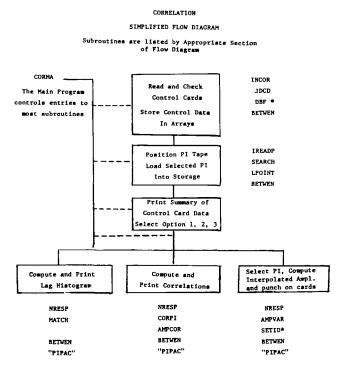
impulse which starts the heart beat is this type of response.

In attempting to apply standard cross-correlations to respiration produced heart period variability called "respiration simus arrhythmia" we have often found small "zero-order" correlations in respiration and heart rate records which by visual inspection, appeared to have strong sinus arrhythmia. These inconsistent findings stimulated us to seek better ways to measure cross-correlation among physiological variables.

Our approach keeps entirely separate the aspects of coincidence, amplitude, and shape. It retains the concept of a response as the primary entity. The first problem is to identify the corresponding responses on a pair of variables.*

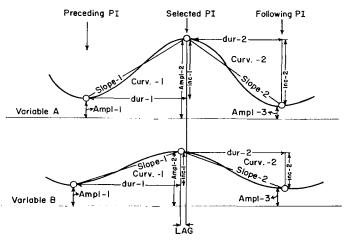
(2) Phases of the Correlation Programs.

The correlation of response parameters proceeds in two Matched PI For Correlation distinct phases (Figures 12, 13, 14).



^{*} GM System Subroutine. "PIPAC" is a FAP coded routine with multiple entries for packing and unpacking parts of PI.

Figure 12

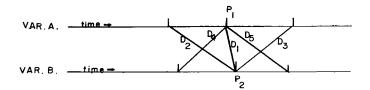


* Ax, A. F.; Zachary, G.; Gudobba, R. D.; Gottlieb, J. S. Psychophysiological data retrieval and utilization. Ann. N. Y. Sci., Vol. 115:

Figure 13

2, pps. 890-904, 1964.

CORRELATION MATCHING METHOD



The PI are indicated by short vertical lines on the time scale of the two variables. P_1 will be matched with P_2 if the time differences D_1 through D_5 meet the following test: D_1 must be less than D_2 , D_3 , D_4 , or D_5 .

Figure 14

During the first

phase, the times of

selected P.I. are matched

and a histogram of the

lags between samples

for the pairs of variables

being matched is printed

out. This enables the

user to select the characteristic

lags for the P.I. he desires to correlate. During the second phase these lags are used as input. The selected P.I. are matched and the subset of those points closest to the specified lags is used for the actual correlations. Matching may take place on either the beginnings or ends of responses as desired.

The input to the program is similar to the P.I. and summary programs previously described and consists of a set of program control cards specifying the desired program parameters and a tape containing the points of interest in the format produced by the P.I. program. Output consists of a summary of control card information plus identification data such as epoch and variable names from the P.I. tape. This is followed by the lag histograms for phase 1 and correlations for phase 2 in convenient tabular form. The program contains extensive optional printout of intermediate data for use in checkout and during early program usage.

III. APPLICATION OF ACQUISITION SYSTEM.

The data acquisition system became operational long before the data processing system did. During this time, considerable data were recorded

by oscillogram and analog magnetic tape. Three physiological variables were analyzed by hand on two studies. The first of these studies has been partially reported previously. (See Ax, Beckett, Fretz, Gottlieb, 1965.)

A. Classical Conditioning of Autonomic Responses in Humans.

1. Rationale.

The notion underlying this study is the concept of learned moti-It is well established that the motives which the individual develops vation. by interaction with his social environment are learned, (Hull, 1943; McClelland, Atkinson, Clark, & Lowell, 1953; Hebb, 1958; Brown, 1961; Miller, 1951; Miller, 1961). The individual learns his motivational pattern uniquely according to his particular endowments and experiences. Since there is almost always more than one motive present, it is necessary to conceive of motives as being organized into a hierarchy in reference to current need, opportunity, and long term consequences. Current need, opportunity and long-term consequences, are very interdependent variables which may interact strongly as illustrated by emotional behavior and impulse buying which after the act may be seen as very inappropriate behavior and to result in undesirable long-term effects. The motivational hierarchy which enables the decision to act (presumably by some sort of reciprocal inhibition) is largely unconscious and may have little relationship to the verbalized conscious "hierarchy of values".

One who tends to be overweight may have placed dieting high on his verbalized hierarchy of values but continue to overeat. The motive to diet is obviously not very high on his hierarchy of motives. This common difficulty in human motivation can be seen to be largely due to the relatively low potency for some people of long-term--as contrasted to short-term--rein-forcements. An immediate threat to health is usually quite successful

for dieting. Clearly to predict and understand behavior the true hierarchy of motives rather than the deceptive verbal "hierarchy of values" must be studied. It is for this reason that the unconscious involuntary physiologic processes are used to study motivation.

The motivational aspect of behavior is believed to be managed by the limbic system of the brain which regulates the autonomic nervous system (ANS). The physiological functions controlled by the ANS thus are prime targets to study with regard to their role in learning motives.

The concept of an aptitude for learning the hierarchy of motives seems strange to some people. Yet few would doubt that the establishment of the hierarchy is learned. Wherever there is learning, we may postulate, there must be an aptitude for the learning. All aptitudes that have been measured appear to be widely distributed in the population and are in general only moderately correlated with each other. Thus we do not expect fo find musical talent, verbal ability and athletic ability to be highly correlated; similarly the aptitude for learning the social motives need not be well correlated with the well-studied aptitudes mentioned above.

Just as educators know that they must adapt their procedures to the intellectual abilities of the student and adjust their expectations for him in terms of his I.Q., so must we learn to recognize and measure the aptitude for learning the social motives and to adapt our social incentives to the person's motivational aptitude and to adjust our expectations of his achievements in terms of his aptitude for learning the social motives.

The aptitude for learning the social motives has a general effect on all achievement, since motivation is a prime factor in all behavior. No matter

how great the talent, if motivation is low there can be little achievement. It would appear that motivational learning is influential for its own acquisition in a regenerative, positive feedback way, thus playing a power factor role. From early childhood relatively small differences in initial motivational aptitude may have profound effects on achievement.

Successful demonstration that these physiological measures of learning correlate with motivational aspects of important life activities such as education, work and family responsibilities would contribute to better scientific description of the mechanism of motivation and to the practical application in selection and training of personnel.

2. Method.

This was a study of clinical group differences rather than one of conditioning per se, hence identical procedure was used on all subjects rather than a procedure employing methodological subgroups for control of stimulus order, pseudo-conditioning, etc. This orientation to clinical group differences makes the study less than ideal for the analysis of the nature of the conditioning obtained. Subsequent studies will be required to clarify these interesting problems.

a. Experimental Procedure.

The experiment was done on each subject over a 5-day period (Figure 15 next page). Five 1-hour sessions of physiological testing were done on consecutive days. The first session was habituation to the laboratory during which 3 different pitched tones were sounded each for 12 seconds for each of 5 trials. The second and third sessions were for conditional training during which two of the tones were reinforced by two different intensities of pain stimuli each 5 times per session. The fourth session

CONDITIONING PARADIGM

DAILY SESSIONS

Habituation 1st cond. 2nd cond.	Extinction	Cold Pressor
-------------------------------------	------------	--------------

A CONDITIONING SESSION

Rest.	Instruction	15 stimuli	Inst.	Rest.	
5'	2'	34'	1"	5'	=47 min.

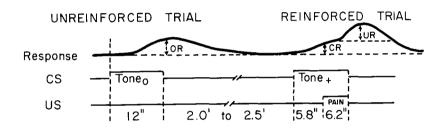


Figure 15

was extinction during which only the tones were given as on the first day. At the completion of the extinction series, the pain electrodes were once more attached and 4 intensities of stimulation (2.5, 3.5, 4.0, and 4.5 ma) were administered at about 3.0-minute intervals so as to enable the determination of the subjects' responsiveness to the pain stimuli when the response was not complicated by a preceding CR elicited by the CS. It was hoped that these responses could be used in a regression equation to adjust for individual differences in response sensitivity so as to reduce the between-subject variance. The pain stimuli can also reveal the systematic discrimination of the response system to incremental pain stimuli.

On the fifth day the cold pressor test was done and 3 I.V. blood samples taken for biochemical analysis being done by Dr. Frohman. The experimental

procedure for each session was preceded by at least 5 minutes recorded undisturbed rest and followed by a 5-minute rest period.

The conditional stimuli used in this experiment were tones of 3 different pitches (470, 770, and 1240 Hz) interrupted (50% on - off 4 times per second at about 75 db loudness. Each tone was presented for 12 seconds for 5 repetitions at pseudo-random intervals (from 2.0 to 2.5 minutes) in 4 sessions on consecutive days. The unconditional stimuli were direct currents applied to the toe pads via zinc sulphate wetted circular sponge electrodes. The direct current values were 2.5 and 3.5 ma; that is, 6.50 and 9.10 ma/cm 2 . An electronic current regulator maintained precisely these current values regardless of skin resistance changes beneath the electrodes. During the first or habituation session each of the 3 tones without the pain was presented 5 times. During the second and third sessions the smaller (2.5 ma) pain stimulus always accompanied the last 6.2 seconds of the middle pitched tone (770 Hz) and similarly the higher pain stimulus (3.5 ma) was always paired with the highest pitched tone (1240 Hz). The lowest pitched tone was never reinforced by pain. On the fourth or extinction session no pain stimuli, only the tones, were presented. This session was identical with the habituation session. Thus during the two conditioning sessions each of the two higher-pitched tones was reinforced a total of 10 times.

Each subject was told for the habituation session that he would hear some tones but he need do nothing. For the two conditioning sessions he was told that some of the tones would be accompanied by a brief pain in his toe which would feel like heat. For the 4th or extinction session he was told that there would be no pain stimuli—that the pain electrodes were not applied to his toe. This true information was given to the subject

in the hope that it would eliminate the random variance caused by varying hypotheses of the subects as to when they might be given pain stimuli. The involuntary autonomic response was of more interest than the conscious expectations.

On the fifth day the subject was required to immerse his foot in continuously stirred ice water for 1 minute. I.V. blood samples were taken before, during, and after the ice water stimulus. During the 10 minutes of stimulation, the maximum rise and fall from the prestimulus resting levels were scored for each variable.

b. Subjects.

Three types of subjects were tested:

- (1) The clinical group consisted of 28 male chronic schizophrenic patients with an age range of 27-41 with a mean age of 31.9 years.

 The mean duration of the illness was 7.6 years with a minimum of over 2 years.

 They were maintained in a special research ward and kept off all drugs for a year or more prior to the time of testing. They were on a good diet and required to participate in a daily program of exercise. According to the diagnosis by a single psychiatrist on a single occasion, their subdiagnoses were distributed as follows: Paranoid 36%, Hebephrenic 18%, Catatonic 14%, Simple 14%, and Undifferentiated 18%. During the 8 years most of these patients have been studied, there have been changes in psychiatric opinion about their subdiagnostic categories; all clinicians agreed, however, that all 28 patients were indeed chronic schizophrenics.
- (2) The control group consisted of 18 healthy employed persons. Each was interviewed by a psychiatrist and rated on the same psychiatric scales on which the patients were rated. In addition the control group was given the Minnesota Multiphasic Personality Inventory, the Wonderlick

Personnel Test, a reversed digits test, and weight and auditory discrimination tests. If any control subject was judged to be unhealthy physically or psychiatrically by the psychiatrist, he was excluded from the control group. The age range was 19 to 44 with a mean age of 28.1 years. There was no attempt to match the two groups on I.Q. Within the control group there was no significant correlation between the GSR conditioning score and the Wonderlick index of I.Q.

c. Physiologic Response Scoring.

Manual analysis was done on skin conductance (SC), skin potential (SP) and finger pulse (FP). The analysis of heart rate, respiration, frontalis muscle tension, face temperature, and ballistocardiogram was postponed until computer analysis could be done.

(1) Base Level.

The palmar conductance and potential were measured prior to the onset of each stimulus and also at five selected points of each (a) During the last minute of the first rest period.

- (b) Between the 5th and 6th stimulus (at the lowest SC point and point of least activity of SP).
- (c) Between the 10th and 11th stimulus.
- (d) Between the 15th stimulus and the instructions for rest.
- (e) Near the end of the final rest period.

Since finger pulse had no calibration, the base level was not considered a useful measure.

(2) The Conditional Responses (CR) to tones (T , T , T) were measured during the habituation and extinction sessions within the 12-

second period while the tone signal was on. During the conditioning sessions the CR was measured only during the 5.8 seconds of the tone prior to the onset of the pain stimulus. The responses to T_0 , T_1 , and T_2 were each measured in the same manner during the conditioning sessions, except those for FP for which the T_{Δ} (unreinforced tone) was measured over the full 12-second tone interval as it was for all variables during habituation and extinction sessions. The purpose of this change was to enable, for one variable, a proper comparison between the unreinforced and reinforced sessions which is not possible when the periods of analysis are of different length. The more obvious solution to this problem would appear to have been to have measured all responses to tones for all sessions only during the first 5.8 seconds of the tone. If this had been done comparisons between tones and between sessions would have all been possible. The reason it was not done was because many of the responses, especially those of FP, had rarely reached their full amplitude at the end of the 5.8 second period; hence, the value obtained at the 5.8 second cutoff was not the best representation of the response amplitude. The data should be rescored both ways to test this hypothesis and to enable all comparisons. Another experimental design which employed unreinforced trials for the usually reinforced tones, T, and T, would, of course, also have provided a solution. This was not done because we feared that less than 100% reinforcement would produce inadequate conditioning in this experiment where the total number of reinforcements was only 10 per tone. Finally it must be reiterated that our primary purpose was the group comparisons rather than a study of conditioning.

(3) The unconditional response (UR) was measured during the 6.2-second period while the pain stimulus was on. In order to make the CR and UR comparable the UR analysis period was not carried beyond the offset

of the pain even though many responses continued to rise after the US offset. The UR are being rescored to examine the full response.

Another problem in comparing the CR and UR is the fact that the UR is nearly always occurring during some phase of CR response or recovery. As mentioned earlier the "Law of Initial Values" is not sufficiently sophisticated to enable correction for this aspect. For some variables and for some stages of the just previous response, the second response may be augmented; for other variables and stages, it may be diminished in amplitude. John Gorham working in our laboratory is investigating this problem.

All responses are calculated by subtracting the amplitude just prior to the beginning of the response from the value either at its maximum or at the end of the analysis epoch as described above.

Skin potential (and heart rate when it is analyzed) presents special problems because it has four typical patterns of response: (a) positive uniphasic, (b) negative uniphasic, (c) positive diphasic (positive portion first), and (d) negative diphasic (negative portion first). The polarity of the response is the potential at the palmar surface referenced to the arm electrode. Normally the palm is negative to the arm reference. No special procedures (such as skin drilling) were used to decrease the resistance at the arm site except the usual washing and rubbing in of electrode paste (Redux). Variable resistance effects between the electrodes and loading was prevented by using an electrometer coupler having over 1000 megohms input impedance. We have determined that at least 10 megohms input impedance is necessary to prevent loading and resistance effect.

The SP measures were taken as follows: (a) frequency of each type, and (b) amplitude of the increments and decrements from both types of responses

whether from uni- or di-phasic responses. In order to avoid scoring as responses the recoveries, only that portion of the secondary wave which exceeded the beginning amplitude was utilized as illustrated below in Figure 16.

Types of Skin Potential and Heart Rate Responses

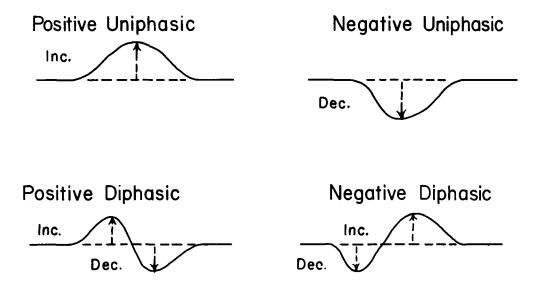


Figure 16

There are problems which require arbitrary solutions. (1) For a response to be counted the change for this study must be at least 0.2 mv in amplitude within 1.0 second. For SC the change must be 0.05 micromho within 5 seconds. (2) If the recovery of a response is not completed when another response of the same polarity occurs the second response must be treated as another response. If the second response reaches a greater value than the first one

(all within the specified analysis epoch), the maximum value of the second response may be used as the minuend from which the amplitude of the variable at the beginning of the first response is subtracted to produce the response amplitude. Such a response is called a cumulative response. (3) The remaining arbitrary consideration is the maximum interval between the maximum or end rise of the first response and the beginning of the second response so as to distinguish between discrete and cumulative responses. This value has been set at twice the time tolerance. For SP it is 2.0 seconds and for SC it is 10 seconds. It should be emphasized that neither frequencies nor amplitude distributions are meaningful nor comparable unless such scoring standards are followed and stated.

There is as yet no clear understanding of the significance of these different types of skin potential responses. Chester Darrow (1964), Robert Edelberg and David Wright (1964), and R. C. Wilcott (1964) have presented tentative explanations but at present no generally acceptable explanation has been presented.

3. Results.

a. Base Levels.

The tendency for the schizophrenic group to have significantly (p < .05) higher average base levels of palmar conductance over all four sessions suggests a higher level of activation (Table 14).

BASE LEVELS*

Variabl	e Hab	First Habituation Conditioning			Second Conditioning Extin		nction 4 Sessions			Cold Pressor		
	С	s	С	s	С	s	С	s	С	s	С	s
SC	2.71	4.18	3.29	4.29	3.54	4.27	2.54	4.03	3.03	4.19	2.63	3.57
SP	-2.6	-14.3	-17.2	-14.9	-18.0	-15.0	-15.8	-12.9	-14.11	-14.16	_	_
SBP	119.7	118.9	120.8	116.3	120.8	120.3	117.8	116.7	119.8	118.1	* 116.4	113.2
DBP	77.3	78.8	77.0	77.3	77.8	80.8	74.9	77.4	76.5	78.5	73.3	73.0

^{*} Middle three samples for each session.

For Schiz Base Level $r_{\rm sc.sp}$ = .26 p > .05 (4 sessions) For Schiz Base Level $r_{\rm sc.sp}$ = .28 p > .05 (4 sessions)

Table 14

The two groups do not differ significantly on SP or BP. It is not known whether higher or lower skin potentials are associated with arousal. But since SP and SC for mean base levels have only insignificant correlations for both control (r = .26) and schizophrenic (r = .28) groups it would appear that SP is not an indicator of the same aspect of arousal that SC is believed to be.

Without valid base level measures for such additional variables as heart rate, peripheral plethysmogram, muscle tension, and EEG desynchronization it would be hazardous to say how the two groups compared on activation or how they adapted over the sessions. As Lacey (1966) has recently pointed out and Darrow (1942), Ax (1953), Sternbach (1960), Lazarus (1966), and others have shown, the physiological indices of activation do not correlate very well. We conclude that activation or arousal is too global and undifferentiated a concept accurately fit the facts. Individuals manifest their activation in unique patterns and do so differently in different situations. Much more research is needed to relate patterns of physiological activation with well described emotional and motivational patterns in many types of individuals.

The correlations between base levels and the various indices of response show a similarly variable pattern. Of the correlations computed on individuals for SC between base levels and response, the range was from zero to .74.

For SP they are equally variable. Such wide individual differences and variability within individuals in regression of response amplitude on base level makes questionable any attempt to remove the base level contribution from response amplitude. There is little to be gained by attempting to apply the "law of initial values", until studies are done which sufficiently

control for the other determinants of response amplitude. The determinants other than base level include individual response specificity, type of arousal and contribution of other variables. Many studies must be done to reveal the true, probably curvilinear, relationship between response amplitude and base level for each variable, each type of stimulus and each "type of subject" (if indeed each individual is not a type unto himself). We come to this lamentable conclusion even though we believe that the contributions of psychophysiology to the study of stress tolerance, motivation and emotional development can be greatly enhanced by the full exploitation of the true "laws of initial values." Much research needs to be done in this area.

b. Orienting Responses.

An important consideration for classical conditioning is for the conditional stimulus originally not to elicit much of an orienting response, or at least to be relatively habituated, before conditional training is begun. Minimal response to the CS prior to conditioning makes it easier to show unambiguously that enhancement in response amplitude or frequency of response has been achieved by the training procedure.

There is uncertainty as to exactly what role the amplitude of the OR has for the course of conditioning. Often it is found that for pseudo-conditioning control groups where there is no pairing of CS with UR the OR habituates whereas for the conditioning groups the OR does not habituate and is said to have become the CR. Some experiments have described increases in latencies as OR became CR and others have even described a third response called the anticipatory response, AR, which occurs just before the US. These varieties of responses are probably influenced by the duration of the CS-US interval, latencies of the response variable, etc. Since our primary

purpose was to describe the differences between two criterion groups rather than detail the intricacies of classical conditioning, we can pursue this problem no further. It is sufficient to note (see Figures 17 to 24, next page) that the healthy control group had larger OR at the beginning of the habituation session but that at the end of the habituation session their mean OR was no larger than that for the schizophrenic group. Thus the conditional response differences between groups cannot be accounted for simply in terms of larger responses to the CS prior to conditioning nor by the OR since the correlations between OR and mean CR are small, averaging .27 for the control group and .21 for the schizophrenic group (Table 15).

ADAPTATION OF ORIENTING RESPONSES

	sc			FP			s_{P_i}		${\sf SP}_d$			
	C	s	P	С	s	p	С	S	р	С	S	P
lst OR - last 3 hab.	. 373	.022	-	12.73	8.02	-	.029	.039	-	281	.020	-
2nd Or - last 3 hab.	. 244	.070	-	14.30	-5.01	-	.253	.004	-	166	.007	-
Comb. OR - last 3 hab.	. 299	.034	∢.01	13.09	-2.11	.01	.122	.018	.05	249	.014	.01

1st OR is the response to the first 3 tones of habituation.

2nd OR is the response to the first tone (T) of first conditioning.

Combined OR is (1st OR + 2nd OR)/2.

Last 3 hab. is the mean of the responses to the last 3 tones of habituation $(T_1 + T_2 + T_3)/3$.

Table 15

The OR habituation
(Table 16) corre-
lates with condition-
ing on the average
considerably better

CORRELATIONS OF OR HABITUATION VS CONDITIONING

	sc	FP	SP _i	$^{\mathtt{SP}}d$
Control (N=18)	.363	.096	.691	.539
Prob	NS	NS	.01	.05
Sch1z (N=28)	.413*	.137	.440	.018
Prob	.02	NS	.02	NS

Orienting Response Habituation is computed by

(E3 First trials/ $_3$ - 3 last trials/3 for habituation + (First trial, T $_1$, lst cond. - E last 3 trials/3 for habituation). The conditioning score is the mean amplitude of CR for first plus second conditioning.

* One subject caused extreme distortion of the distribution requiring a non-parametric Rank Difference correlation. Product moment r = .789.

Table 16

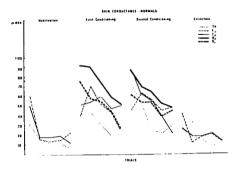


Figure 17

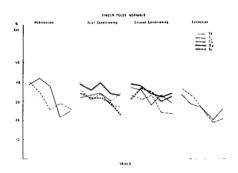


Figure 19

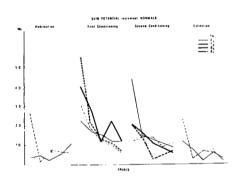


Figure 21

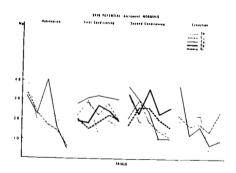


Figure 23

L

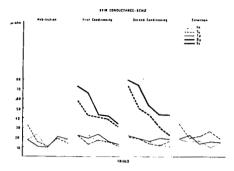


Figure 18

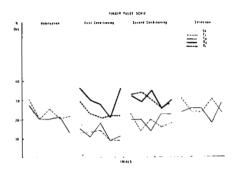


Figure 20

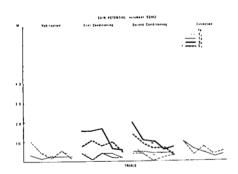


Figure 22

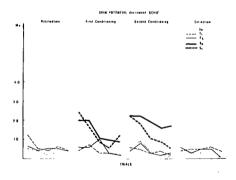


Figure 24

for controls (.419) than for schizophrenics (.252).

It could be that two factors are involved here. The higher initial OR for the healthy group may represent a greater sensitivity to their environment and their rapid habituation could be considered as conditioning. Conditioning in the general sense is modification of a response with experience and may include decreases as well as increases. The role of the OR ("sensitivity to stimuli not yet classified as to relevance") in conditioning is not well understood, although it could be argued that for a stimulus to become a successful conditional stimulus, it must be taken cognizance of (responded to) in some manner by the organism. It is unknown to what extent an organism will develop a sensitivity to a previously totally ignored stimulus by associative conditioning.

c. Unconditional Responses.

A second important consideration for conditioning is for the unconditional stimulus (US) to elicit an adequate unconditional response (UR). Reference to Figures 17-24 and Tables 17

	sc				FP			${\tt SP}_i$			sp _d		
CR	С	S	p *	С	S	₽*	С	s	p*	С	s	p*	
Habituation	.21	.17	NS	28,44	27.55	NS	.68	.50	NS	2.11	.55	.01	
1st Conditioning	.49	,16	.01	31.98	11.47	.01	1.58	. 34	NS	2.79	.53	.01	
2nd Conditioning	. 54	.16	-01	31.12	18.90	.01	1.58	.41	.05	2.11	- 48	.01	
1st & 2nd Condit.	. 52	.16	.01	31.89	15.06	. 01	1.67	. 38	.05	2.47	. 51	.01	
Extinction	.20	.18	NS	29.99	40.71	NS	.79	. 50	NS	1.72	.42	.01	
UR													
1st Conditioning	.63	.47	. 05	32.59	24.60	NS	2.24	1.10	.05	2.06	1.44	NS	
2nd Conditioning	.58	. 51	NS	33.82	31.34	NS	1.12	1.01	NS	2.51	1.69	. 05	
1st & 2nd Condit.	.61	.48	.05	32.56	28.63	NS	1.68	1.07	NŞ	2.21	1.58	NS	

RESPONSE AMPLITUDES

Amplitudes for the habituation and extinction sessions are means of responses to all tones. Amplitudes for the conditioning sessions are means of the responses to the reinforced tones (T and T 2), and means of the responses to the unconditioned stimuli (S and S 3).

Table 17

^{*}Kruskal-Wallis one way analysis of variance.

					PERCENT	RESPONS	E FREQUEN	ICY					
and 18			sc			FP			${\tt SP}_i$			SP,	ı
	CR	c	s	p*	С	s	p*	С	s	n*	С	s	r*
shows that	Habituation 1st Conditioning	72.7 93.7	59.6 59.1	NS .00003	70.0 93.1	65.9 43.1	.00003	20.3 18.1	28.3 17.1	NS NS	67.1 81.2	39.3 39.9	.0013
both the	2nd Conditioning 1st & 2nd Condit, Extinction	91.7 93.2 66.0	61.2 59.8 61.1	.00016 .00003 NS	89.4 91.1 71.1	63.3 53.2 69.8	.00003	24.2 21.0 20.5	18.5 18.0 28.0	NS NS NS	70.1 74.3 57.1	42.9 41.3 35.6	.0008 .00004 .0228
•	. UR												
amplitude	lst Conditioning 2nd Conditioning 1st & 2nd Condit.	96.5 90.9 93.7	90.2 84.5 87.6	NS NS NS	94.6 92.8 93.6	78.6 86.9 83.0	.0217 NS .0113	35.0 24.4 29.2	23.7 27.3 25.2	NS NS NS	63.8 70.5 67.8	65.2 59.0 62.2	NS NS NS
and fre-	ist a znu condit.	73.7	87.0	n _o			. SUBTYPES		23.2	1.5	07.5	02.2	15.5
quency of	CR		tive U	niphasic S		itive [iphasic S		ative U C	niphasic S		ative I	Diphasic S
UR appear	Habituation let Conditioning 2nd Conditioning let & 2nd Condit.	18 21 19	.5	28.3 17.1 15.3 16.3	2	.6 0 .8	0 0 3.2 1.6	6 4 5	2.6 1.9 6.0 3.7	33.3 33.2 32.5 33.0	1 2 2	4.5 9.4 4.1 0.6	6.0 6.7 10.4 8.3
adequate	Extinction UR	17	.4	27.5	3	.1	.5	4	7.6	30.0		9.5	5.6
for the	lst Conditioning 2nd Conditioning 1st & 2nd Condit.	20	.8 .6 .4	23.7 22.1 22.6	3	.2 .9 .8	0 5.2 2.6	3	9.4 19.4 0.6	46.2 44.4 45.8	3	4.4 31.1 17.2	19.0 14.6 16.4
two groups.	Percent response from and extinction sessions (T, and T,), a	lons. Fo	r the	ondition:	ing sessi	ons the	percent						
No sub-	*Mann-Whitney U test					•	•						
iest						Т.	ahla	18					

ject Table 18

failed to provide UR. The correlations between parameters of CR and UR are very low (.01 to .21) which suggests that if some minimal UR is present, it suffices for conditioning.

d. Conditional Responses.

The most remarkable finding is the greatly reduced mean conditional responses for the schizophrenic group as shown in Tables 17 and 18. Appropriate probability tests of these group mean differences indicate it is highly improbable (p < .01) that these differences could be due to chance. The percent of cases correctly classifiable by these scores indicate several individual scores to be highly diagnostic, thus indicating the autonomic conditional approach may have considerable power as a diagnostic test.

e. Tone Discrimination by CR.

The response discrimination between the reinforced tones $(T_1,\ T_2) \ \ \text{and the unreinforced tone} \ \ (T_0) \ \ \text{shows essentially no discrimination}$ for the schizophrenic group and only moderate discrimination by the normal

group (Figure 25, Table 19).

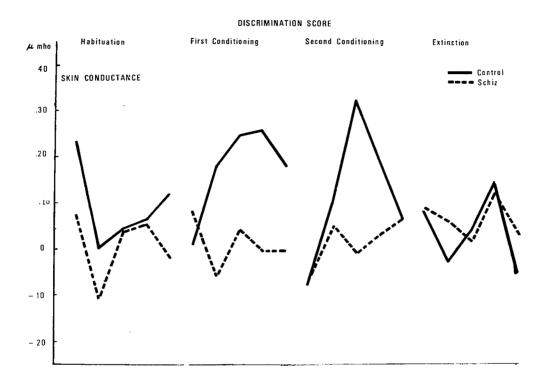


Figure 25

		sc		FP			SP;			$\mathtt{SP}_{\vec{d}}$		
	С	s		С	s		c	s		С	s	
Habituation	.08	.01	.05	9.31	.17	.05	. 22	03	.05	.10	.21	NS
First Cond.	.17	.02	.01	-5.79	-6.07	NS	.08	.00	NS	. 58	.06	.05
Second Cond.	.11	.02	NS	-7.68	-6.37	NS	.11	07	NS	.18	03	NS
First and Second Cond.	.14	.02	.01	-6.52	-5.47	NS	.13	02	NS	. 38	.02	.01
Extinction	.03	.05	NS	1.23	1.88	NS	01	.17	NS	.25	.21	NS

DISCRIMINATION SCORES

Discrimination Score = $(T_1 + T_2)/2 - T_0$

The curves do not suggest any im.

provement in discrimination with increasing trials after the middle of the first

Table 19

conditioning session. Any discrimination that had developed during the rein-

forced period promptly disappeared when reinforcement was omitted in the extinction session.

The significantly greater discrimination demonstrated by the control group shows that at least a part of the conditioning superiority of the control is due to discriminative learning and not mere sensitization as could be claimed for the greater frequency and amplitude of the CR since there was no control for pseudo-conditioning.

f. Variance in Latencies.

Still another measure of response to the CS is the variance in latency. If the responses of a subject have a significantly smaller variance than would be expected by chance to randomly selected periods where no experimental stimuli were given, it is demonstrated that at least some of his responses measured during the stimulus are elicited by the stimulus.

Since the latencies to an imaginary random stimulus would have a uniform random distribution the theoretical variance would be:

$$\sigma^2 = (\alpha - \beta)^2/12$$

where α is the lower boundary and β the upper boundary of the range. Since our conditional stimulus period was 5.8 seconds the theoretical variance is 2.83. It was found for GSR latencies of CR for 8 trials selected for best discrimination between groups by GSR CR amplitude that the 18 normal subjects had significantly smaller than chance variance in latency whereas only 13 of 23 of the schizophrenic patients had such small latencies (variances were not computed for five subjects who had less than three responses).

This finding suggests that about half of the patients were not responding to the tones significantly more than chance. One can confidently conclude that at least these subjects and those with too few responses did

not condition probably because their responsiveness to the CR was too small or inconsistent to enable conditioning. On the other hand those who had significantly smaller than chance variance in latency do not by that fact alone demonstrate conditioning. Their responses to the tones could mean only that they were continuing to make orienting responses to the CS with neither normal adaptation of the OR nor with any enhancement due to conditioning. Without additional control groups for pseudo-conditioning for which the CS and US are given but not paired, it is impossible to distinguish between "true conditioning" and sensitization or failure to habituate the OR.

g. Combined Scores.

By combining several of the conditioning measures (Table 20,

SUMMATED SCORES										
	Σ React.	Σ Cond.	Σ Disc.	Σ CP	Σ Tot					
Cont.	.459	.939	.505	.715	.656					
Schiz.	295	602	352	470	431					
Diff.	.753	1.541	.857	1.185	1.087					
Prob.	< .02	< .01	< .01	< .01	< .01					
Reactivit	y = (1) Mean F	P _{dec} and SC in	c to 4 pain sti	muli at end of	extinction +					
	(2) Total	FP and SC res	ponse to T , S	and T , S for	r 1st and 2nd					
	condit	ioning +								
	(3) FP dec	rement plus S	C increment dur	ing CP session.						
condition	ing = SC + FP	+ SP _{dec} CR am	plitude + FP _d %	frequency for	1st and 2nd					
	conditioning.									
Σ Disc = $(T_1 + T_2)/2 - T_0$ for 1st and 2nd conditioning for SC and SP_d .										
Σ CP = (HR.	+ SC, + BC,)	- (DBP, + MT,	+ # GSR) for C	old Pressor.						

Table 20

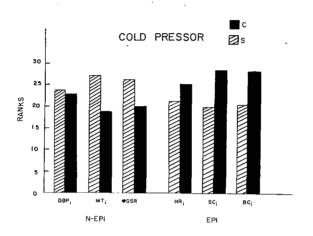


Figure 26

which best distinguish between the two groups it is possible to classify 87% of the total group correctly with only 3 normals and 3 patients misclassified. This is the same percent correct classification as for the single best conditioning score which implies that the autonomic conditioning is similarly reflected in all 3 variables. Probably much of the variance not common to these conditioning variables is due to error.

However if we add to the conditioning scores an index obtained from the physiological response scores to the cold pressor test (Table 21,

		REST			INC			DEC
	С	s	P	c	S	P	c	S p
HR	63.4	70.0		30.0	26.8		8.0	6.1 N.S.
SBP	116.4	113.2		17.6	21.3	N.S.		-
DBP	73.3	73.0		14.3	14.8	N.S.	-	-
BCG	.79	.75		26.2%	16.9%	.05	23.22	21.4%
FP	.43	.40		8.8%	41.4		76.3%	63.1% .01
sc	2.63	3.60	N.S.	4.06	2.65	.01	-	-
€ GSR	.59	1.18	N.S.	2.15	1.02	.01	-	-
RR	15.9	15.1		5.3	5.4	N.S.	- 3.6	2.0

COLD PRESSOR SCORES

Table 21

Figure 26) done on the fifth day of testing we find the number of misclassi-

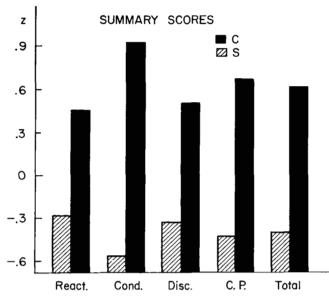


Figure 27

fied subjects reduced to one control and one patient. A review of these two misclassified subjects confirms the patient to be clearly a chronic schizophrenic with no signs of improvement. The case history of the control subject does reveal some difficulties in gaining emotional maturity with one

severe psychiatric breakdown but currently he is functioning well. Obviously our measures contain enough error to readily permit this much failure in classification even if our basic variables were primary to schizophrenia which as yet is quite unconfirmed. It is to be expected that upon replication these combined best discrimination scores would inevitably regress somewhat in their diagnostic power.

As yet we have not had an opportunity to utilize the response amplitudes to standard pain stimuli as possible correction modulators for the conditional responses, but they are included in Table 22 as a basic part of the findings.

BASE LEVELS AND RESPONSES TO 4 PAIN STIMULI FOLLOWING THE EXTINCTION SESSION

Stimulus Intensity		Skin Con	ductance		Finger Pulse					
	Control N=11			ophrenics =21		trol 13	Schizophrenics N=21			
ma	Base (umho)	Response (umho)	Base (umho)	Response (umho)	Base (mv)	Response (% Change)	Base (mv)	Response (% Change)		
2.5	2.85	.53	4.25	.93	15.2	32.5	19.1	42.4		
3.5	2.71	74	4.41	1.02	16.5	34.3	21.8	49.1		
4.0	2.59	1.18	4.42	1.27	15.8	39.1	21.8	51.6		
4.5	2.62	1.37	4.44	1.35	17.2	36.8	19.8	52.3		

Table 22

Other aspects of a battery for best discrimination between two groups should include: (1) an increase in the range of difficulty of the items so as to optimally test each subject regardless of his aptitude; (2) to optimize the test item combinations by the discriminant function; (3) to replicate on new and larger groups; and (4) to purify or subdivide the groups into more homogeneous categories. This last notion of subdivision is very important. There are usually several mechanisms by which an individual copes with his problems. Some of these mechanisms such as "passivity" and "aggressiveness" which might serve fairly well by themselves, in combination may elicit maximum retaliatory reaction from the environment and cause great distress. Such incompatible or conflictual mechanisms may exist at the psychological (behavioral), physiological, and biochemical levels. Our test profiles must take into consideration these various styles of adjustment.

Simple linear combinations suitable for only monotonic variables such as the linear discriminant function cannot do this. The general finding that samples of schizophrenic patients nearly always have a wider range than normal on nearly all tests strongly suggests that two or more mechanisms are involved in their disability. The first step usually made in the attempt to recognize this heterogeneity is to classify schizophrenics into two groups on the basis of some variable. The presence or absence of a blood serum factor (Frohman, et al., 1961) or nor-epinephrine-like response to stress (Funkenstein, et al., 1957; Ax, 1953) are examples. Since such variables can operate in combination with still quite unknown results, they need to be simultaneously recorded and utilized together. This multiple variable team approach is being attempted at The Lafayette Clinic. Although we had in common a substantial group of schizophrenic patients on whom we

can intercorrelate our variables, our control groups were not in common and thus our comparisons are incomplete.

h. Non-Schizophrenic Low Motivation Subjects.

In order to test our hypothesis that low aptitude for autonomic conditioning should have profound relationships to social maladjustment other than schizophrenia we attempted to test a sample of skid row habitues who have a life history of low social motivation. Only four of these were successfully recruited, demonstrated to be free from physical and psychotic pathology and who would come into the hospital for two weeks for the diagnostic workup and psychophysiological testing. The scores analyzed on these show very similar results to those found for the schizophrenic group. The conditioning scores were as low or lower than for schizophrenia and the unconditional response to the pain stimulus was lower for skin conductance but essentially normal for finger pulse. Base level for skin conductance was low, BP was high. There were many circumstances such as age, alcoholism, chronically poor diet, etc. that make these subjects unsatisfactory. These were the main reasons why more were not tested.

Instead we undertook a research program (with Department of Labor assistance) to study students in the vocational retraining schools most of whom were school dropouts and adults who have had a long history of low achievement. These subjects will be classified as to evidence of motivation and also compared to other groups comparable with regard to race, education, socio-economic origin, I.Q., personality variables, age, etc., but who differ markedly with regard to achievement and social motivation.

B. Physiological Concomitants of Psychological Differentiation.

The results of the conditioning experiment indicated there was relatively little autonomic discrimination between the three tones. The question was raised as to what subject characteristics might relate to the discrimination variable. Mr. Courter and Dr. Watttenmaker were graduate students in psychology at Wayne State University and also were research assistants in our laboratory. They designed this experiment (Courter, Wattenmaker and Ax, 1965) to relate the cognitive style of "field independency" with autonomic differentiation. Field independency was measured by a "closure flexibility test" a form of imbedded figures test, and a "verbal concept attainment test". Forty normal college students served as subjects and were grouped into relatively higher and lower field independency. The group having the greater field independency very significantly (p < .01) better discriminated the tones by their GSR responses. "This study demonstrates that the stimulus generalization gradient involves an interaction between the cognitive style of the organism and the impinging stimuli, not merely the quantitative physical characteristics of the stimuli". These findings further suggest that the field dependent person may have a functionally less well-differentiated autonomic nervous system.

More research will be required to describe the functional relationships between perceptual discrimination and autonomic differentiation and the role learning plays in both, and their interactions.

IV. Conclusions.

The desirability of utilizing the digital computer for processing psychophysiological data is more obvious than ever. This study has clarified somewhat the problems in doing so and the specifications required for a practicable system. The difficulties which we experienced were due to an underestimation of the magnitude of the task and an over-estimation of our engineering resources. The best approach now (1967) would appear to be the use of an on-line type of computer with integral A/D and D/A converters and sampling under computer program control. Both analog and digital tape storage should be provided as backup when the computer is not available during data acquisition or when more computing is required than can be done in real time or when much less computing is required than real time requires so as to enable the computer to use its full speed potential by tape speedup.

Signal conditioning, including automatic editing by pattern recognition and less exotic methods, should be done both by analog and digital methods at various stages of the signals' progress through the system. An optimum compromise between early on-line analog signal conditioning and later digital manipulation must be worked out so as to maximize signal/noise ratio under the constraints of engineering and apparatus costs, signal distortion (such as lags due to analog filtering), digital computer speed, computing costs and time available. The nature of the variable, the parameters desired from it, and the local situation with regard to engineering sophistication, apparatus, and funds available all enter the compromise equation.

Sampling rates and resolutions should be kept to a minimum required to provide the information desired since the cost of digital computing is

roughly proportional to the number of bits to be processed. Flexible sampling rates under computer program control can often save a great deal of computing time.

The system must be easily calibrated by the regular operator of the acquisition system on a daily basis or more frequently if necessary.

Ideally where small drifts cannot be avoided a calibration signal for the variable which it calibrates should be periodically updated (manually or automatically) and carried along with the signal and made available to the computer program which should be able to normalize the computed values to the standard calibration. Time code event mark and ID mark must be provided for both polygram and magnetic tape and a tape search system provided so as to locate any record, event, or time on the analog record.

Ideally, these codes should be automatically converted to appropriate digital values so as to avoid human work and error. It might appear that the above recommendations are merely obvious good engineering practice. In the practical laboratory situation, however, numerous compromises must be made. We have found the above considerations to be essential minimal requirements that cannot be ignored.

Our computing programs have not been used enough to provide the experience necessary for any conclusions or recommendations beyond the rationale for their design. The response approach and correlations among parameters of responses matched for minimal variance in lag appear to be a useful and theoretically valid approach.

The findings that the parameters of autonomic conditioning and the epi-norepi-like physiologic response patterns have great diagnostic

power indicates the method is well worthy of further study and application to other groups of interest. While there is still much to be learned by the classical conditioning method of autonomic processes in humans, the instrumental method may prove even more fruitful. Classical conditioning with laboratory stimuli may fail to involve the basic motives sufficiently to tap the significant aspects of human life. Instrumental conditioning which makes the reinforcement contingent on the physiologic response, on the other hand, is more potent in getting involvement. It also appears to be a better fit with natural real-life learning. Accordingly, a next logical step in the development of physiological indices of stress tolerance, motivational aptitude and emotional development should involve instrumental conditioning of autonomic processes.

Finally an area of motivation as much in need of clarification as the aptitude for motivational learning is that of <u>current motivation</u>. All performance tasks including intelligence, personality and aptitude tests, as well as our own tests of motivational aptitude, are influenced by the <u>current motivation</u> as they are by the aptitude under test. It would be of great value to have an index of current motivation independent of the performance and of antecedent conditions such as instructions, deprivations, or promises. We have made this investigation our highest priority for our next study. During a standard tracking task which serves as the criterion of motivation the physiological parameters of arousal will be monitored during several intensities of positive (money and visual feedback) and negative (pain) reinforcement. Conflictual motives and anxiety will also be investigated to determine whether they have

characteristic physiological patterns which can be identified and removed from the physiological indices of the arousal related to the criterion performance. The characteristic physiological patterns of pleasant and unpleasant reinforcement will be a very interesting byproduct of this study.

These studies can be of value to NASA and the theory of human motivation by demonstrating and describing some of the relationships between physiological response and the motivation aspect of performance efficiency. To the extent that positive results are obtained, the prediction equations can indicate how indices of physiological response can be used to monitor the motivation being brought to bear on performance and learning.

REFERENCES

- Ax, A. F. The physiological differentiation between fear and anger in humans. Psychosom. Med., 1953, 433-442.
- Ax, A. F. Goals and methods of psychophysiology. <u>Psychophysiology</u>, 1964, 1, 8-25.
- Ax, A. F. Electronic storage and computer analysis. In Venables, P., and Martin, Irene (Eds.) Manual of Psychophysiological Methods.

 Chapter 14: pp. 481-519. Amsterdam: North Holland Publishing Co., 1967.
- Ax, A. F., Beckett, P. G. S., Cohen, B. D., Frohman, C. E., Tourney, G., & Gottlieb, J. S. Psychophysiological patterns in chronic schizophrenia. In J. Wortis (Ed.), Vol. IV. Recent advances in biological psychiatry. New York: Plenum Press, 1962.
- Ax, A. F., Singer, S. J., Zachary, G., Gudobba, R. D., Gottlieb, J. S.

 Psychophysiological data retrieval and utilization. Ann. N. Y.

 Acad. Science, 1964, 115: 890-904.
- Ax, A. F., Andreski, L., Courter, L. R., DiGiovanni, C., Herman, S., Lucas, D., and Orrick, W. The artifact problem in telemetry of physiological variables. In Murry, W. E. and Salisbury, P. F. (Eds.), Biomedical sciences instrumentation. N. Y.: Plenum Press, 1964, 229-233.
- Ax, A. F., Beckett, P. G. S., Fretz, N. A., & Gottlieb, J. S. Development of a selection test for motivational aptitude. NASA Contractor Report No. 156. National Aeronautical & Space Administration, Washington, D. C., January, 1965.

- Courter, R. J., Wattenmaker, R. A., and Ax, A. F. Physiological concomitants of psychological differentiation. <u>Psychophysiology</u>, 1965, <u>1</u>: 282-290.
- Darrow, C. W., Jost, H., Solomon, A. P., & Mergener, J. C. Autonomic indications of excitatory and homeostatic effects on the electroencephalogram. <u>J. Psychol.</u>, 1942, <u>14</u>: 115-130.
- Darrow, C. W. The rationale for treating the change in galvanic skin response as a change in conductance. <u>Psychophysiology</u>, 1964, <u>1</u>: 31-38.
- Edelberg, R., & Wright, D. J. Two galvanic skin response effector organs and their stimulus specificity. <u>Psychophysiology</u>, 1964. <u>1</u>: 39-47.
- Frohman, C. E., Latham, K. L., Warner, P., Beckett, P. G. S., & Gottlieb,

 J. S. Biochemical identification of schizophrenia. Arch. Gen.

 Psychiat., 1961, 4: 404.
- Funkenstein, D. H., King, S. H., & Drolette, N. E. <u>Mastery of Stress</u>.

 Cambridge, Mass.: Harvard Univ. Press, 1957.
- Lacey, J. I. Somatic response patterning and stress: some revisions of activation theory. Chapt. 2, pp. 14-37. In Appley, M. H. and Trumbull, R. <u>Psychological Stress</u>. New York: Appleton-Century-Crofts, 1967.
- Lazarus, R. L. <u>Psychological stress and the coping process</u>. New York:

 McGraw-Hill. 1966.
- Sternbach, R. A. Two independent indices of activation. <u>Electroencephal</u>.

 <u>Clin. Neurophysiol.</u>, 1960, <u>12</u>: 609-611.
- Wilcott, R. C. The partial independence of skin potential and skin resistance from sweating. <u>Psychophysiology</u>, 1964, <u>1</u>: 55-66.

Table 2

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517	2065 205											2070								
519	2065 206.											1978								
521	1974 197											5103								
523 525	2081 207 2057 2051											1976								
527	1964 200											2010 2128								
529	2046 2046											1976								
531	2008 200											1902								
577	1974 1976											1970								
535	1978 1920											1886								
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543	1852 185											1942								
545	1966 1966											1894								
547	2069 2070											2051								
549	2006 2006											5094								
551	2233 222											2234								
553 555	2129 2123 2101 2097											2149 1997								
557	2088 208											2081								
559	2053 2046											2075								
561	2199 219	3 2189	2160	2093	2088	2089	2087	2091	2088		2094	2088	2089	2068	2103	2095	2099	2101	2199	2096
563	2105 2101											2261								
565	2117 2111											2014								
567 565	2095 2071											2091 2020								
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573	2073 2069											2131								
575	2167 2160											2044								
577	216C 2151											2081								
579 581	2034 2034 2097 2053											2162 2099								
583	2172 2169											2139								
585	2205 2200											2145								
587	2191 2184											2073								
589	1982 1988											2078								
591	2017 2026	5 2024	2021	2024	2022	2020	2021	2024	5,18		2075	5069	2071	2073	2069	2º 64	2068	2071	2071	70.64
593 595	2215 2227											2175								
597	2026 2026 2140 2137											1998								
599	2038 2038											2269								
601	2267 2259										2148									
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633	2057 2056	2055	2048	2109	2124	2124	2123	2128	2123		2133	2123	2125	7895	7789	2079	2083	2085	2085	2079
635	2089 2087										2006									
637	1927 1946										1906									
639	1900 1902	1900	1858	1900	1848	1940	1937	1941	1918		1940	1 7 18	1444	1442	LAUR	14/0	14/4	1491	450	17/4

Table 2, Contd.

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515	7216 7237 7239 7279 7264 7291 2301 2288 7785 7299	2305 7293 7789 7309 2798 7773 7770 7291 7798 2775
517	2273 2293 2300 2254 2277 2233 2241 2231 2230 2241	2249 2739 2251 2289 7301 2281 2282 2305 2309 2291
519 521	2791 2311 2309 2289 2284 2296 2305 2292 2289 2300 2297 2315 2323 2310 2307 2318 2324 2311 2309 2341	2309 2277 2263 2281 2287 2271 2268 2288 2297 2288 2363 2355 2354 2371 2375 2354 2352 2372 2373 2291
523	7771 7285 7789 7275 7267 7281 7791 2273 7743 7747	2255 2241 3237 2254 2261 2240 2241 2288 2307 2289
525 527	2289 2309 2311 2297 2293 2308 2395 2275 2269 2281 2277 2296 2305 2291 2290 2391 2309 2297 2293 2309	2293 2277 2273 2291 2391 2281 2275 2293 2391 2280 2320 2305 2297 2316 2341 2331 2327 2341 2363 2333
529	7333 7350 2361 2309 7745 7244 2752 2737 2731 2743	2256 2242 7239 2255 7762 2243 2740 7257 7768 7249
53 53 3	2746 2243 2325 2315 2310 2323 2333 2323 2317 2339 2521 2544 2556 2542 2532 2540 2553 2551 2559 2575	2405 2411 2411 2426 2434 2416 2416 2435 2467 2503 2588 2577 2571 2586 2597 2581 2517 2344 2299 2269
535	7765 7779 7789 7777 2265 7183 2150 2128 2117 2128	2141 2127 2122 2069 1980 1938 1930 1949 1956 1938
537 539	1936 1937 1828 1773 1757 1768 1782 1770 1763 1777 1510 1518 1530 1516 1510 1524 1537 1477 1441 1446	1762 1666 1631 1641 1650 1629 1624 1642 1652 1550
541	1386 1406 1414 1406 1399 1410 1475 1408 1402 1415	1460 1442 1434 1459 1469 1495 1384 1398 1499 138H 1434 1426 1419 1435 1445 1425 1419 1434 1449 1446
543	1462 1481 1492 1479 1468 1479 1494 1486 1502 1523	1542 1526 1518 1539 1543 1526 1523 1561 1584 1568
545 547	1562 1580 1590 1577 1567 1582 1600 1590 1581 1594 1594 1613 1624 1652 1683 1703 1724 1711 1701 1713	1606 1594 1582 1601 1611 1590 1585 1602 1619 1598 1730 1717 1704 1705 1712 1693 1685 1703 1715 1700
549	1694 1714 1742 1731 1725 1735 1749 1734 1729 1740	1760 1786 1798 1817 1830 1813 1804 1818 1831 1814
551 553	1810 1826 1841 1830 1822 1831 1847 1839 1829 1838 1845 1859 1867 1852 1842 1854 1870 1857 1846 1857	1858 1845 1832 1844 1854 1838 1834 1852 1866 1849 1876 1876 1875 1893 1996 1890 1883 1898 1913 1895
555	1886 1886 1892 1874 1864 1877 1892 1882 1874 1886	1938 1937 1926 1941 1954 1934 1926 1945 1961 1962
557 559	1972 1993 2006 1994 1986 1993 2010 2002 1994 2009 1965 1977 1990 1977 1966 1973 1990 1998 2021 2042	2029 2016 2006 2021 2032 2016 2010 2026 2014 1977 2064 2047 2034 2048 2061 2043 2037 2060 2084 2069
561	2064 2079 2092 2016 2066 2077 2096 2065 2034 2040	2061 2044 2034 2046 2063 2051 2045 2083 2101 2085
563 565	2079 2093 2106 2089 2080 2089 2104 2121 2131 2147 2087 2100 2109 2098 2089 2103 2117 2099 2091 2101	2165 2151 2139 2151 2165 2151 2142 2116 2111 209; 2122 2107 2096 2109 2123 2121 2128 2149 2168 2153
567	2147 2160 2173 2161 2151 2133 2131 2113 2104 2115	2172 2117 7036 71 7 7173 7121 7126 7144 7168 2131
569 571	2050 2065 2079 2087 2097 2114 2133 2124 2113 2121	2139 2127 2121 2172 2195 2193 2175 2195 2211 2192
573	2184 2159 2207 2187 2175 2188 2235 2195 2181 2191 2192 2225 2247 2233 2221 2236 2253 2238 2227 2239	2211 2203 2183 2193 2205 2190 2183 2197 2211 2197 2261 2258 2247 2260 2274 2257 2252 2271 2285 2268
575	7760 7733 2279 7713 2199 2210 2276 2715 7707 7711	2193 2145 2125 2138 2153 2137 2128 2146 2163 2143
577	2042 2063 2006 1992 1978 1990 2004 1994 1988 1933 1522 1529 1545 1533 1518 1530 1550 1541 1510 1448	1775 1710 1686 1698 1710 1692 1682 1699 1690 1562 1446 1433 1422 1437 1451 1436 1425 1441 1386 1313
581	1294 1308 1326 1310 1294 1306 1326 1314 1402 1319	1337 1320 1308 1318 1333 1318 1313 1321 1297 1267
583	1753 1769 1285 1774 1260 1269 1289 1254 1194 1190 1099 1114 1130 1117 1105 1115 1134 1118 1102 1111	1206 1194 1181 1192 1210 1193 1186 1190 1148 1110 1133 1118 1106 1118 1134 1118 1110 1114 1114 1090
587	1084 1058 1116 1100 1086 1100 1118 1090 1070 1078	1096 1085 1068 1084 1101 1078 1038 1045 1058 1041
589 591	1032 1046 1066 1054 1042 1046 1062 1051 1040 1048 1034 1049 1066 1056 1058 1076 1097 1084 1073 1081	1069 1054 1044 1062 1074 1041 1028 1046 1066 1046 1103 1093 1085 1084 1089 1070 1054 1074 1094 1077
593	1066 1081 1097 1091 1100 1116 1137 1124 1114 1123	1143 1130 1122 1129 1138 1119 1112 1126 1146 1129
595 597	1122 1136 1180 1215 1216 1230 1250 1239 1224 1234 1212 1227 1258 1257 1246 1258 1278 1265 1254 1266	1257 1246 1218 1218 1230 1214 1202 1216 1234 1221 1287 1265 1246 1257 1275 1257 1242 1259 1278 1265
599	1262 1286 1305 1292 1289 1240 1310 1247 1291 1298	1318 1307 1797 1314 1332 1313 1304 1317 1334 1321
601 603	1314 1320 1322 1305 1286 1298 1320 1305 1293 1302 1336 1357 1378 1365 1349 1358 1378 1366 1354 1365	1325 1322 1317 1334 1350 1334 1323 1339 1361 1345 1384 1348 1325 1336 1354 1338 1325 1339 1358 1339
605	1293 1754 1310 1294 1279 1287 1312 1301 1289 1286	1298 1286 1270 1282 1299 1281 1271 1285 1305 1260
607	1272 1731 1249 1235 1217 1276 1249 1238 1240 1270	1298 1789 1775 1291 1307 1789 1778 1794 1793 1761
611 611	1745 1759 1782 1770 1254 1762 1783 1778 1778 1793 1311 1325 1342 1330 1315 1326 1351 1346 1334 1345	1313 1302 1285 1297 1318 1306 1294 1316 1340 1322 1368 1357 1340 1354 1373 1355 1333 1342 1362 1365
613	1334. 134H 1366 1355 133H 1333 134H 1334 1320 1332	[352 1339 1326 1339 1368 1354 1346 1361 1382 1369
615 617	1359 1370 1388 1398 1390 1402 1422 1408 1393 1403 1414 1429 1449 1438 1422 1433 1452 1442 1430 1440	1427 1415 1400 1412 1430 1415 1405 1418 1441 1429 1461 1450 1435 1450 1470 1453 1439 1452 1473 1458
614	1438 1449 1468 1457 1440 1450 1474 1462 1445 1457	1476 1462 1447 1462 1480 1446 1454 1470 1522 1516
621 623	1506 1522 1542 1526 1510 1519 1546 1537 1519 1528 1544 1557 1577 1564 1549 1553 1563 1549 1537 1546	1548 1537 1519 1532 1549 1534 1527 1548 1572 1555 1566 1552 1537 1549 1569 1559 1554 1571 1594 1579
625	1565 1578 1596 1582 1570 1564 1571 1557 1542 1553	1566 1577 1577 1544 1564 1574 1574 1571 1574 1574 1574 1574 1567 1569 1564 1597
621 629	1586 1600 1618 1630 1629 1642 1665 1654 1641 1651	1674 1663 1651 1664 1681 1663 1649 1662 1685 1672
631	1662 1667 1678 1662 1644 1653 1672 1661 1648 1660 1674 1686 1702 1691 1675 1685 1706 1694 1676 1641	1690 1690 1677 1693 1716 1695 1682 1698 1719 1694 1701 1690 1681 1690 1706 1690 1678 1695 1721 1710
633	1702 1714 1732 1718 1702 1713 1734 1722 1704 1713	1730 1716 1701 1713 1734 1718 1708 1698 1699 1681
637	1670 1686 1702 1689 1677 1689 1694 1669 1654 1562 1632 1646 1666 1649 1621 1623 1642 1630 1613 1625	1685 1670 1657 1670 1688 1650 1628 1643 1662 1646 1649 1641 1596 1578 1590 1574 1560 1578 1597 1581
639	1561 1542 1560 1534 1518 1526 1547 1537 1523 1513	1502 1482 1464 1477 1493 1478 1468 1485 1490 1463

Table 2, Contd.

TIME						VARIABLE	NO. 12						
515 519			6 1393 1397 3 1390 1394		1394 1392			1390 1394				1390 1394 1386 1388	
523			A 1384 1390		1388 1386			1384 1388				1391 1394	
527			6 1393 1398		1399 1397			1400 1404				1402 1405	
531 535			n 1409 1414 3 1442 1451		1414 1414			1420 1425				1426 1430	
539			4 1492 1498		1497 1496			1497 1502				1500 1502	
543	1502	1496 150	1496 1502	1499	1499 1496	1499 1498	1500	1492 1498	1493	149R	1493 1497	1490 1490	1488
547			1482 1486		1484 1482			1477 1480				1472 1474	
55) 555			1464 1470 4 1450 1454		1464 1462			1458 1462				1456 1458 1446 1459	
559			R 1442 1446		1442 1439			1434 1442				1434 1438	
563			H 1434 1442		1440 1438			1438 1446				1441 1444	
567 571			6 1438 1446 6 1440 1446		1442 1440			1438 1446				1442 1446	
575			2 1479 1486		1486 1483			1430 1442				1493 1502	
579			1510 1572	1523	1528 1528	.1537 1534	1538	1521 1517	1500	1494	1490 1474	1470 1468	1467
583			2 1458 1462		1463 1462			1475 1486				1490 1496	
587 591			5 1505 1514 2 1602 1608		1522 1524			1544 1555				1580 [588] 1621 [624]	
595			7 1621 1626		1626 1618			1618 1622				1614 1620	
599			8 1614 1618		1616 1610			1606 1610				1602 1606	
607			6 1602 1606 6 1590 1594		1604 1598 1597 1585			1590 1596 1582 1587				1589 1594 1 1579 1586	
611			5 1582 1584		1582 1576			1574 1574				1566 1572	
615	1570	1564 1566	5 1562 1566	1560	1564 1558	1564 7557		1557 1560			1556 1558	1550 1558	1550
619	1556	1548 1550	1548 1548	1546	1549 1542	1548 1542	1548	1541 1544	1540	1542	1538 1542	1534 1540	1534
623	1539	1533 1534	1530 1532	1528	1531 1524	1528 1522		1522 1525				1517 1523 1	
627			1518 1521		1521 1514			1514 1515				1506 1510 1	
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515	51 H	905	910	920	910	908	926	915	913	892		109	
527	902	896	915	49 B	1478 908	1177	1352 913	956 930	1556 918	908 1221		1597 913	
539 551	90 <i>2</i> 930	90H 910	910 926	301	913	917 917	914	910	915	_ 904		899	
563	907	914	906	910	921	941	90.5	918	942	907	905	896	
575	902	899	906	4061	910	913	915	924	934	974 924		914	
587 5 99	921	91 <i>7</i> 916	908 914	924 928	918	926	934	904	912	916		928	
611	901	913	918	906	907	921	908	908	914	934	963	1061	
623	94 A	944	945	954	1018	1000	914	921	930	913	905	914	
635	918	910	915	913	934	907							
TIME						VAR(ABLE	NO. 27						
515	1804	180	1807	1806	1808	1897	1804	1808	1800	1797	1798	1798	
527	1798	1 800	1802	1798	1795	1804	1798	1794	1794	1794	1798	1895	
539	1810	1809	1810	1819	1810	1809	1808	1877	1805	1896		1810	
551 563	1810 1809	1814 1809	1812	1812 1809	1810 1808	1812 1805	1812 1806	1812 1807	1812	1812		1812	
575	1801	1802	1812	1877	1834	1841	1848	1862	1862	1866		1878	
587	1842	1886	1887	1884	1876	1874	1872	1870	1868	1869		1864	
599	1864	1866	1864	1864	1864	1864	186C 1843	1860 1840	[862 [842	1862 1836	1862 1834	1959 1936	
611 623	1857 1833	1854 1828	1848 1826	1846 1824	1849 1826	1846 1826	1847	1826	1826	1828	1826	1822	
635	1824	1826	1830	1430	1834	1832			2				

#1 1511	ING FOR	10 04/52020	6010	VAR	1	HEART PERIO	D IN SECONDS
-TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURY
421.0	EE	0.90	0.	1110.0	EE	1.03	0.
427-0	BEP	0.93	0.	1110-1	HI	1-06	0.50
422.4	H E	0.96	0.35	1111.2	BEP	1.05	0.
424-1	LÜ	0.92	-0.16	1111.9	EF	1.00	-0.14
426.2	HI	66.0	0.55	1115.6	8F	1.00	0.
426-9	LG	0.12	-0.26	1115.9	f.O	0.97	-0.77
427.8	EEP	0.98	O.	1117.0	EEP	1.06	0.
429-0	ВĿ	1.00	0.	1117.0	BEP	1.06	0 •
571.0	EE	1.04	0.	1118.0	ΗI	1.19	0.32
572-0	BEP	0.59	0.	1121.5	FO	0.94	-0.51
572.5	1.0	0.99	-0.51	1122.8	EEP	0.99	0.
5 -0	HI	1.00	0.51	1124.0	88	1.01	0.
5 6-5	ĽΩ	1.00	-0.59	1230.0	EE	0.99	0.
5 7-0	HI	1.05	0.69	1231.4	BEP	0.97	0.
577.8	EEP	1.02	0.	1231.9	LO	0.95	-0.31
577-8	BEP	1.02	0.	1233.0	HI	1.01	0.56
578.5	1 0	0.98	-0.35	1234.6	LO	0.97	-0.29
580.0	1.4	1.07	0.43	1237.0	HI	1.05	0.55
580.4	FF BR	1.03	-0.21	1237.2	EEP BE	1.03	0. 0.
582.4	EFP EFP	1.45	0.	1239.0 1304.0	EE.	0.99 0.97	0.
585.0	BE	1.05		1305.4	BEP	0.91	0.
705.0	E E	0.48	0.	1300.2	LO	0.90	-0.54
706.6	BEP	1.04	0.	1367.2	HI	0.97	0.39
707.0	HI	1.05	0.66	1309.5	ŁO	0.92	-0.41
709.3	LG	J.98	-0.35	13/1.2	EEP	1.01	0.
710.3	FR	1.04	0.11	1371.2	BEP	1.01	ō.
712.4	EEP	1.33	0.	1373.0	HI	1.07	0.55
712-4	BEP	1.33	0.	1375.5	LO	0.98	-0.48
715.9	₿E	1.04	0.	1377.0	Ηſ	1.04	0.55
716.5	LS.	1.00	-0.80	1377.0	EEP	1.04	0.
718.0	ΗI	1.36	0.28	1378.0	ВE	1.00	0.
718.0	FEP	1.05	0.	1484.0	EE	0.97	0.
719.0	ВE	1.00	0.	1445.5	LO	0.93	-0.47
#55.O	t.F	0.97	0.	1485.8	BEP	0.97	0.
856.4	BFP	1.03	0.	1487.0	ΗI	1.00	0.59
857.0	ΗI	1.03	0.57	1486+6	LO	0.92	-0.40
857.6	L L	0.98	-0.15	1491.6	EEP	1.01	۵.
859.0	нt	1.63	0.43 -0.16	1493.0	BE EE	1.04	0.
859.5	Ld	0.98		1635.0	HI	0.94	0.
862-2	EEP BEP	1.05 1.05	٠.	1635.3 1636.0	REP	0.98 0.98	0.19 0.
862.2 864.0	HI	1.07	ა. 0.31	1536.1	EF	0.95	-0.16
865.6	E.F	1.00	-0.32	1640.5	BR.	0.94	0.18
867.6	89	1.00	0.32	1641.8	FEP	1.09	0.
868.0	H.i	1.09	J. 76	1641.8	BEP	1.09	0.
0.868	f F P	1.09		1642.0	HI	1.09	0.51
869.0	дr.	1.05	ė.	1643.5	LÜ	1.02	-0.63
577.0	£ E	0.93	0.	1645.0	ΗI	1.08	0.69
978.4	BÉP	3.45	₩.	1645.5	LO	1.06	-0.29
979.2	HI	0.99	0.42	1647.0	1H	1.09	0.40
981.4	16	9.44	-0.05	1647.0	EEP	1.07	0.
984.2	EEP	1.00	(· •	1649.0	BE	1.04	C •
986.0	₿E	1.12	C.	1769.5	€€	0.98	0.

Table 3. Heart Period in Seconds.

	!	CINTS OF INT	EREST SUMMARY				
ESSILA NU U415	2020010 TN	ME CCON	IKOL) ID 0317	TESTED MAKCH	5, 1964	SECOND CONDI	TIONING
AKIABLE 1	HEART PERIOD IN	SECONDS		SUMMARY NO	1	6 P	DINTS OF INTERES
FCCH 2	112						
	BEG EPUCH	572.0	END EPOCH	577.8		DURATION	5.8
	BEG AMP	0.99	AT TIME	572.0 577.8			
	MAX AMP	1.06	AT TIME	575.0			
	MIN AMP	0.99	AT TIME	572.5			
***************************************	MEAN AMP	1.02	STAN DEV				
100.0	PER CENT GOOD I		O. PER CENT L			PER CENT'S	HORT EDIT
	INIT AMP	INCREMENT	DURATION	SLOPE	CURV	LATENCY	PREC DRIFT
INST INTERVAL	0.99	-0.01	0.5	-0.01		0.	
ESPCASE 1	C.99	0.08	2.5	0.03	0.51	0.5	0.
ESPENSE 2	1.06	-0.07	1.5	-0.05	-0.59	3.9	
ESPENSE 3	1.00	-0.04	0.5	0.13	0.69	4.5	
ESSICN NO 0475	2020-010 N.		TROL) 10 0317	TESTED MARCH			TIONING
FLCH 3	152						
	BEG EPCCH	577.8	END EPOCH	583.6		DURATION	5.8
	BEG EPCCH	1.02	AT TIME	577.8		DONATION	
	END AMP	1.05	AT TIME	583.6			
	MAX AMP	1.07	AT TIME	580.0			
	MIN AMP	C.98	AT TIME	578.5			
	PEAN AMP	1.04	STAN DEV	0.03			
100.0	PER CENT GOOD	DATA	O. PER CENT L	ONG EDIT	0.	PER CENT S	HORT EDIT
	INIT AMP	INCREMENT	DURATION	SLOPE	CURV	LATENCY	PREC DRIFT
IKST INTERVAL	1.02 C.98	-0.04 C.09	0.7	-0.06 0.06	0.43		
		-0.03	0.4	-0.08	-0.21	2 2	
ESPENSE 2 AST INTERVAL	1.07	0.00	1.2	0.00	-0.21	4.6	
. FJI INIEKVAL	1.03	0.00	1.4	0.00		T • O 1	

Table 4. Heart Period in Seconds - 6 Points of Interest.

AMPL

9.05

4.22

3.57

8.63

7.92

7.62

8.09

7.95

7.80

6.52

6.52

3.95

3.31

6.81

6.66

7.40

6.55

6.55

3.62

3.75

10.89

11.23 10.79

10.09

10.69

10.02

11.07

10.20

7.14

10.49

9.96

9.91

11.27

10.18

10.18

4.92

4.46

PAGE

CURV

0.

0.

0.

0.

0.

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0.

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0.

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0.

-0.50

-0.55

0.

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9.

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-0.34

0.

0.

0.

0.

0.61

0.48

0.49

0.26

-0.41

.0.26

TYPE

EEP

ВE

TIME

1122.8

1124.0

CURV

С.

C.

Ú.

(.

O.

0.

0.

AMPL 6.45

6.10

TYPŁ

FE

HEP

TIME

421.0

422.0

986.0

1110.0

1111.2

1117.0

1117.0

BE

FΕ

BEP

EFP

PFP

5.26

9.00

4.05

6.32

6.33

CURV

0.

0.

0.

0.

ο.

-0.21

0.47

TIME

1775.8

1781.5

2329.6

2329.6

2335.6

2337.0

SEP

BEP

EEP

BE

TYPE

BEP

EEP

AMPL

3.49

3.33

1754.7

1770.0

1771.1

1775.0

Finger Pulse in Percent Full Range - Var. 3 Table 5.

9.64

9.75

9.05

10.01

Lυ

ΗI

BEP

FFP

PCINTS OF INTEREST SUMMARY

SESSIEN NO 04/52020	10010 N	AME (CUNTRO	L) 10 0317 T	ESTED MARCH 5	1964 SEC	OND CONDITION	ING
MARIAELE 3 FING	ER PULSE IN P	ERCENT FULL R	ANGE	SUMMARY NO	1	3 POINTS	OF INTEREST
EFECE 2	112						
		572.0	END_EPUCH	577.8		DURATION	5.9
	EG AMP	8.73	AT TIME	572.0			
	NE AMP	7.45	AT TIME	577.8			
	AX AMP	9.09	AT TIME	574.3			
	IN AMP	7.05	AT TIME	577 . 8			
r	EAN AMP	0.45	STAN DEV	0.75			
100.0 PER	CENT GUOJ DAT	۸)	. PER CENT LU	NG EDIT	n. 0	ER CEN T SH OPT	roit
					CURV	EATENCY DRE	C Dalet
FIRST INTERVAL	c./3	C . 26		0.13		^ .	
LAST INTERVAL	9.05	-1.45	3.0	-(·48		? • ዛ	
SESSILN NG C4752C20		NTS OF INTERE	SE SUMMARY L) 10 0317 T	ESTED MARCH 5	, 1964 SEC	RMO COMPILIAM	I vid
VERTABLE 3 FING	ER PULSE IN F	EKCENT FULL R	ANGE	SUMMARY NO	1	1 POINT	S OF INTEMEST
EFLCF 3	152						
	EG EPUCH	577.8	FND EPUCH	583.6		DURATION	5 • q
	EG AMP	7.65	AT TIME	577.8			
	AMP UN	4.24	AT TIME	583.6			
	CAX AMP	7.65	AT TIME	577.8			
	IN EMP LAN AMP	4.24 4.24	AT TIME STAN DEV	583.6 0.			
•	EAR AMP	4.44	STAN DEV	0.			
100.0 FER	CENT GOOD DAT	Α 0	. PER CENT LU	NG EDIT	Ŏ• b	FR CENT SHORT	FD[T
		-			CURV		CORIET
FIRST INTERVAL	1.65	-3.40	5.8	-0.59		0•	
LASI INTERVAL	4.24	0.	0.	0.		5.A	

Table 6. Finger Pulse in Percent Full Range - 3 Points of Interest.

PI LIST	ING FOR	ID 0475202	01040	VAI	R 12	SKIN POTEN	TIAL IN MILL	IVOLTS			PAGE 5
TIME	TYPE	AMPL	CUR V	TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV
421.0	EE	-8.16	J.	980.0	BR	-7.78	0.	1649.0	BE	-10.99	0.
422.0	BEP	-7.57	0.	982.0	EK	-9.85	0.30	1769.0	E E	-1.41	0.
474.4	BR	-8.53	0.	984.2	EEP	-9.95	0.	1770.0	8EP	-1.32	Ŏ.
427.8	EEP	-10.99	J.	986.0	8E	-10.80	0.	1773.2	BR	-1.87	0.
429.0	НE	-11.18	0.	1110.0	EE	-2.50	0.	1775.8	EEP	-3.33	0.
571.0	FΕ	-8.16	0	1111.2	BEP	-2.50	0.	1775.8	BEP	-3.33	0.
572.0	bFP	-7.78\	0.	1113.4	BR	-2.60	C •	1781.6	EEP	-8.34	0.
572.4	E۴	-7.64	-0.62	1117.0	EEP	-6.01	0.	1783.0	B€	-9.71	
574.4	8R	-7.63	0.	1117.0	BEP	-6.01	0.	1918.0	EE	-2.64	0.
575.8	ER	-9.85	0.60	1120.0	ER	-8.91	0.52	1919.0	BEP	-2.60	0.
577.8	FEP	-10.14	0.	1122.0	BR	-9.38	0.	1920.8	BSE	-2.41	0.
577.8	BEP	-10-14	0.	1122.d	FEP	-10.42	0.	1921.8	8R	-3.10	0.
578.4	BR	-10.19	0.	1124.0	ВE	-11.09	0.	1922.6	ER	-3.65	0.50
581.0	ΗI	-12.33	0.55	1230.0	ЕE	-3.15	0.	1923.0	ESE	-4.06	0.
582.6	FF	-9.00	-0.62	1231.4	BEP	-2.96	0.	1924.8	EEP	-3.93	0.
583.6	EEP	-8.53	0.	1237.0	BR	-4.06	0.	1924.8	3EP	-3.93	0.
585.0	BÉ	-4.62	0.	1237.2	EEP	-4.25	0.	1925.4	5R	-4.11	0.
705.0	EE	−7. ೮೮	0.	1234.0	вE	-5.26	0.	1930.6	EEP	-7.41	0.
706.2	۴ĸ	-8.44	0.32	1364.0	EΕ	-1.23	0.	1932.0	B.F.	-8.20	0.
706.6	HEP	-8.49	G.	1365.4	BEP	~1.55	0.	2068.0	EE	-1.68	0.
708.8	нĸ	-8.72	0.	1355.6	ER	1.87	0.29	2069.0	BEP	-1.96	0.
712.4	FEB	-12.14	0.	1358.2	BR	-2.14	0.	2072.4	8R	-2.05	0.
712.4	HFP	-12.14	0.	1370.6	ER	-4.43	0.55	2074.8	EEP	-3.05	0.
715.4	Iн	-14.21	0.59	1371.2	EEP	-4.43	0.	2074.8	BEP	3.05	0.
716.0	FF	-13.10	-0.49	1371.2	BEP	-4.43	0.	2081.0	EFP	-7.97	n.
718.0	нR	-13.29	0.	1373.0	BR	-4.76	0.	2082.0	9.E	-8.72	. 0.
718.0	ł FP	-13.29	J.	1377.0	EEP	-9.10	0.	2188.0	EE	-3.05	0.
719.0	Вē	-14.16	û.	1378.0	BE	-9.76	` 0.	2189.6	BEP	-2.87	0.
855.0	EG	-6.80	0.	1494.0	EE	-1.32	0.	2192.4	BR	-3.51	0.
856.4	8E2	-0.52	ა.	1445.8	BEP	-1.00	0.	2193.8	ER	4.06	0.43
855.0	BR	-6.85	٥.	1488.6	BR	-1.77	0.	2195.4	EEP	-4.11	0.
862.2	FEP	-9.38	0.	1491.6	EEP	-3.33	С.	2197.0	BE	-4.16	0.
867.2	REP	-9.38	0.	1493.0	ВE	-3.79	0.	2322.0	EE	0.31	0.
864.6	НI	-11.33	0.53	1635.0	EE	-0.78	0.	2323.8	BEP	0.35	0.
866.C	LG	-10.33	-0.45	1636.0	BEP	-0.87	0.	2326.4	BR	-0.01	0.
868.0	EEP	-11.14	0.	1638.8	BR	-1.14	0.	2329.6	EEP	-1.87	0.
869.0	HE	-11.57	0.	1641.8	EEP	-3.15	0.	2329.6	BEP	-1.87	0.
977.C	FÉ	-8·20	0.	1641.8	BEP	-3.15	0.	2335.6	EEP	-7.22	ņ.
978.4	BE2	-7.97	0.	1647.8	EEP	-9.10	C.	2337.0	9 E	-7.59	2.

Table 7. Skin Potential in Millivolts - Var. 12.

PCINIS OF INTEREST SUMMARY

SESSIEN NU U4	1520206010	NÂME J		TESTED MARCH	5, 1964	SECOND CONDIT	TONING
VARIABLE 12	SKIN PUTENTIAL	IŅ MILLIVGE	T.S.	SUMMARY NO	1	5 P(DINTS OF INTEREST
EFLCF Z	112						
	EEG EPUCH BEG AMP END AMP MAX AMP MIN AMP MEAN AMP		END EPOCH AT TIME AT TIME AT TIME AT TIME STAN DE	572.0. 577.8 572.4 577.8		DURATION	_, 5 • 8
100.0	PER CENT GOOD	UATA	O. PER CENT	LONG EDIT	0.	PER CENT SH	IORT FOIT
FIRST INTERVAL RESPLASE I LAST INTERVAL	1N11 AMP -7.18 -1.83 -4.85	INCREMENT 0.14 -2.03 -0.28	DURATIUN 0.4 1.4 2.0	SLUPE 0.35 -1.45 -0.14	CURV 0.60	LATENCY 7. 2.4 3.4	PREC DRIFT

POINTS OF INTEREST SUMMARY

SESSIEN NO 047520206010	NAME (CUNT	KUL) 10 0317	TESTED MARCH	5, 1964 9	SECOND COMPLI	TIONING
VARIABLE 12 SKIN PUTENTIA	L IN MILLIVELTS		SUMMARY NO	1	4 Pr	TINTS OF INTEREST
EFCCF 3 152						
BEG EPUCH BEG AMF END AMP MAX AMP MIN AMP MEAN AMP	577.6 -10.14 -8.53 -8.53 -12.33 -10.01	END EPOCH AT TIME AT TIME AT TIME AT TIME AT TIME STAN DE	577.8 583.6 583.6 581.0 1.69	c.	OURATION PER CENT SI	5.A 40RT FOIT
INII AMP FIRST INTERVAL -10.14 RESPENSE 1 -10.19 RESPENSE 2 -12.33 LAST INTERVAL -9.00	INCREMENT -0.05 -2.14 3.33	OURATION 0.6 2.6 1.6	SLOPE -0.08 -0.82 2.08 0.47	CURV 0.55 -0.62	LATENCY 0.6 3.2 4.8	PPFC DRIFT

Table 8. Skin Potential in Millivolts - 3 Points of Interest.

TIME	TYPE	AMPL	CURV	FIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV
421.0	£ E	24.98	0.	864.0	EF	25.63	-0.50	1491.6	EEP	23.88	0.
422.0	BEP	24.98	0.	d58.3	ВR	24.61	0.	1493.0	BE	23.44	0.
427.8	FEP	24.98	o.	468.0	EEP	24.61	0.	1635.0	EE	24.91	0.
429.0	ВF	24.03	J.	859.0	βE	93.96	0.	1636.0	BEP	22.70	0.
571.0	F£	20.92	0.	977.0	££	24.91	O.	1641.0	BSE	23.37	0.
572.0	BEP	24.63	U.	478.4	REP	24.16	0.	1641.8	EEP	23.37	0.
577.0	PSE	24.32	J.	934.2	EÉP	24.03	С.	1641.8	вEР	23.37	0.
577-8	EEP	24.40	0.	630.0	BE	23.88	0.	1643.0	ESE	23.59	0.
577.8	BEP	24.40	ე.	1110.0	EE	22.48	ç.	1647.8	EEP	24.61	n.
579.0	ESF	24.51	ા.	1111.2	BEP	23.50	9.	1648.0	BR	24.83	0.
587.6	EEP	20.00) .	1115.0	∃SE	24.25	ာ •	1649.0	3E	51.49	0.
584.0	HR	29.15	J.	1117.0	ĿĿ₽	23.88	n.	1769.0	E E	23.14	0.
585.0	BF	95.32	J.	1117.0	4.EP	23.88	0.	1770.0	BEP	23.44	9.
705.0	F.F	23.74	Ð.	1118.0	ESE	23.44	0.	1775.0	8.6	24.18	0.
706.6	BEP	25.34	3 •	1122.8	EEP	24.25	0.	1775.8	EFP	24.18	0.
711.0	BR	20.13	Ú.	1123.0	88	24.18	0.	1775.8	ŖĘ₽	24.18	0.
111.0	BSĒ	26.13	. •	1124.0	BE	79.03	C •	2068.0	FE	25.05	0.
12.4	EEP	51.76	0.	1230.0	EΕ	24.32	ί.	2069.0	4Ep	25.34	ე.
717.4	REP	59.16	U.	1231.4	8EP	24.18	U •	2074.0	BSE	25.49	ე.
713.0	ESF	70.44	ñ.	1237.2	EEP	23.83	0.	2074.8	EEP	26.21	0.
713.0	нı	73.44	r.50	1238.0	BP	25.56	0.	2074.8	BEP	26.21	0.
715.0	t: F	21.21	-0.69	1239.0	BE	30.84	O.	2076.0	F S E	27.35	9.
718.0	Вĸ	25.17	0.	1304.0	EE	24.83	r.•	2081.0	BR	27.49	0.
718.0	EEP	25.77	J.	1365.4	BEP	24.61	0.	2081.0	EEP	27.49	0.
719.0	вE	75.46	٥.	1370.0	BSE	24.91	0.	2032.0	8 E	90.94	0.
855.0	FF	24.83	მ•	1371.2	EEP	23.96	0.	2138.0	EE	23.74	ĵ.
856.4	BEP	23.96	Ú •	1371.2	ЯEР	23.96	0.	2189.6	BED	24.91	0.
861.C	BR	24.40	c.	1372.)	£SE	23.29	C.	2195.4	EEP	25.34	0.
861.0	BSE	24.40	0.	1377.3	BR	23.29	0.	2197.0	ВF.	.25.34	0.
862.2	FEP	29.60	C.	1377.0	EEP	23.29	0.	2322.0	EE	23.14	ő.
862.2	BEP '	29.60	U.	1378.0	BE	75.39	0.	2323.8	BEP	23.51	n.
863.0	FSE	32.44	C.	1454.0	EE	25.05	j.	2328.0	BE	23.14	9.
863.C	н	32.94	0.50	1485.8	BEP	23.37	Ů.				•

Table 9. Muscle Tension in Microvolts.

POINTS OF INTEREST SUMMARY

		PULKIS CF INT	CREST SUMMART				
SESSION NO CAT	צבנבננטונ	NAME (CON	TKOL) 10 C317	TESTED MARCH	1 5, 1964	SECOND CONDI.	FIUNING
VAKLAELE 25	MUSCLE TENSTO	N IN MICKEVELT	S	SUMMARY NO	1	3 0	DINTS OF INTEREST
EFCCF 2	112						
	MAX AMP	512.C 24.C3 24.40 24.40 24.C3 24.25	END EPOC AT TI AT TI AT TI AT TI STAN 1	ME 572.0 ME 577.8 ME 577.8 ME 572.0		DURATION	5 • 8 ·
80 • €	FER CENT GOOD	DAIA	O. PER CEN	LONG EDIT	13.	8 PFR CENT SI	HORT FOIT
FIRST INTERVAL	24.03	INCRÉMENT 0.37 0.	DURATION 5.8 0.	SLOPE 0.06 0.	CURV	LATENCY O. 5.9	PREC DRIFT
	•	PCINTS OF INT	EKEST SUMMAKY				
SESSIEN NO 047:	ežtztotlů	NAME (CÚN	1kGL) 10 0317	TESTED MARCH	. 5, 1964	SECOND CONDIT	TONING
VARIABLE 23	MUSCLE TENSION	IN MICKEVULT	S	SUMMARY NO	1	2 PC	INTS OF INTEREST
EFECF 3	152						
	DEG AMP	577.6 24.40 28.00 28.06 24.40 26.34	ENJ EPUC AT TIM AT TIM AT TIM AT TIM STAN C	E 577.8 E 583.6 E 583.6 E 577.8		POTTAPUG	5 . 8
79.3	PER CENT GLOD	ΑΤΑ	O. PER CENT	LONG EDIT	20.	7 PER CENT SE	IDRI EDII
FIRST INTERVAL	INII AMP 24.40 28.00	1ncrement 3.66 3.	DURATIUN 5.8 0.	SLGPE 0.63 0.	CURV	LATENCY C. 5.8	PREC DRIFT

Table 10. Muscle Tension in Microvolts - 3 Points of Interest.

TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV
421.0	E٤	3.64	0.	1112.0	BSE	3.40	0.	1775.8	вEР	3.06	0.
422.0	HEP	3.03	U.	1114.0	ESE	3.34	0.	1777.0	BR	3.08	0.
426.0	ЯK	3.68	n.	1114.0	ĹΟ	3.34	-0.48	1781.6	€€P	3.25	0.
427.8	FEP	3.73	ο.	1117.0	EEP	3.41	C •	1783.0	BE	3.29	0.
429.0	86	3.75	ű.	1117.0	3EP	3.41	0.	1918.0	FE	3.07	0.
571.0	FE	3.60	0.	1122.0	BSE	3.ol	C •	1919.0	BEP	3.07	0.
572.0	HEP	3.61	0.	1122.3	EEP	3.61	0.	1920•0	BSE	3.07	0.
577.C	BR	3.62	٥.	1124.0	ESF	3.60	0.	1923.0	ESF	3.07	0.
577.8	EEP	3.66	0.	1124.0	нE	3.60	0.	1924.8	ΕĒΡ	3.11	0.
577.8	HEP	3.00	0.	1230.0	€E	3.25	0.	1924.8	BEP	3.11	0.
583.6	EEP	3.71	0.	1231.4	вЕР	3.26	0.	192 7. C	BK	3.11	0.
585.0	Hr.	3.75	0.	1237.2	EEP	3.29	ე.	1930.6	EEP	3.21	0.
7C5.0	٤F	3.57	0.	1239.0	ðЕ	3.36	¢.	1932.0	BE	3.26	0.
706.6	вEР	3.50	J.	1364.0	ΕE	3.16	C •	2068.0	£E	2.88	9.
711.0	88	3.60	o.	1365.4	HEP	3.16	0.	2059.0	BEP	2.89	0.
717.4	EEP	1.67	C.	1369.3	BR	3.20	0.	2074.8	EEP	2.91	0.
712.4	REP	3.07	0.	1371.2	EEP	3.26	0.	2074.8	SEP	2.91	0.
714.0	EEP	3.43	() •	1371.2	BEP	3.26	0.	2076.0	9.R	2.92	ე.
719.0	BE	3.83	0.	1377.0	EEP	3.42	C.	2081.0	ECP	3.13	0.
855.G	FE	3.48	0.	1378.0	вE	3.43	0.	2082.0	8 F.	3.21	0.
856.4	aee	3.48	0.	1484.0	ΕE	3.07	0.	2188.0	EE	2.91	n.
860.0	BR	3.51	0.	1485.8	BEP	3.09	0.	2189.6	BEP	2.90	0.
862.2	₽₽₽	3:59	0.	1491.6	EEP	3.14	n.	2192.0	H!	2.98	0.03
862.2	HEP	3.09	0.	1493.0	3E	3.16	ე.	2192.0	BSE	2.98	0.
868.0	EEP	3.06	О.	1635.0	EE	3.03	0.	2194.0	ESF	2.90	9.
869.0	BE	3.00	0.	1630.0	BEP	3.02	C.	2195.4	EEP	2.89	ე.
977.0	f. f.	3.42	6.	1041.8	EEP	3.02	0.	2197.0	ßΕ	2.91	9.
978.4	BEP	3.45	G.	1541.8	BEP	3.02	ο.	2322.0	EΕ	2.82	0.
982.0	BSE	3.00	C •	1044.0	вĸ	3.08	0.	2323.8	8EP	2.78	0.
984.0	ESE	3.56	0.	1547.5	EEP	3.28	0.	2329.6	EEP	2.82	0.
984.2	EFP	3 . 56	C •	1549.0	ВE	3.34	0.	2329.6	HEP	2.82	0.
986.0	BE	3.57	٥.	1759.0	EE	3.03	0.	2331.0	BR	2.86	0.
1110.0	£έ	3.34	0.	1770.0	BEP	3.04	c.	2335.6	EEP	3.07	0.
1111.2	REP	3.35	ű.	1775.3	EEP	3.06	е.	2337.C	BE	3.09	0.
1112.0	111	3.43	0.25								

Table 11. Skin Conductance in Micromhos.

PUINTS OF INTEREST SUMMARY

SESSILN NO 047	sztátotlo	NAME (CENT)	(UL) ID 0317	TESTED MARCH	5, 1964 S	ECOND CONDITIO	ONING
VARIABLE 27	SKIN CLNOULTAN	CE IN MICKOMHOS	5	SUMMARY NO	1	3 POII	NTS OF INTEREST
EFLCF 2	112						
	DEG EPUCH BEG AMP END AMP MAX AMP MIN AMP MEAN AMP	572.C 3.61 3.66 3.66 3.61 3.03	END EPOCH AT TIME AT TIME AT TIME AT TIME STAN DE	572.0 577.8 577.8 572.0		DURATION	5 . 8
100.6	PER CENT GOOD	ATAU	O. PER CENT	LUNG EDIT	0.	PER CENT SHOP	RT FOIT
FIRST INTERVAL LAST INTERVAL	۱NIT AMP غ.61 ع.دد	INCREMENT C.O1 C.O5	DURATION 5.0 0.8	SLUPE 0.00 0.06	CURV	LATENCY F	PREC DRIFT

1	1 1	IC	4(1	INI	レレビ	C T	CHMEAUV

SESSIEN NO 0475202	10010	NAME (CCN	1 KUL) [D 0317	TESTED MARCE	ዛ, 5 ₄ , 1964	SECOND CONDITI	LONING	
ANTARLE ST 2VT	A CLINCUCTAN	CE IN MICROME	6S	SUMMARY NO	1	1 PO1	INTS OF INTERF	ST
EFLCF 3	152							
	EEG EPUCH DEG AMP END AMP MAX AMP MIN AMP MEAN AMP	577.8 3.66 3.51 3.91 3.66 3.91	END EPOCI AT TIM AT TIM AT TIM AT TIM CTAN DI	577.8 583.6 583.6 577.8		DURATION	5.8	Ī
LCU.C PER	CENT GUUD I	DATA	O. PER CENT	LONG EDIT	0.	PER CENT SHO	ORT EDIT	
FIRST INTERVAL	1N11 AMP 3.06 3.91	INCREMENT C.25 C.	DURAT 10N 5.8 0.	SLOPE 0.04 0.	CUR V	LATENCY 9. 5.8	PREC DRIFT	

Table 12. Skin Conductance in Micromhos - 3 Points of Interest.

Conversion of Data Logger Units to Physiological Values

The following formula is used to convert data logger units to physiological units: $Y = A + BX + CX^2 + DX^3$ where X = Data Logger Units (range 0 to 4095 for + 10 volts)

and Y = Physiological Units.

The conversion values for each variable are as follows:

		A	В	С	D
Heart Period (seconds)	=	11063	+.000542299		
Finger Pulse Amplitude (% total range)	=	_2.03070	+.004868120		
Finger Skin Potential (MV)	=	48.5797	031005	~.0000057979	+.0000000013476
Integrated Muscle Potential (μV)	#	-66.842	+.132097	000039165	+.0000000048841
Smoothed GSR (µmhos)	=	-5 .17890	+.004039820	+.000000449881	

Conversion of Voltage Changes as Recorded on the Polygraph to Changes in Physiological Units

By means of the following relationships it is possible to determine the amount of change in physiological variables from the fluctuations in voltage recorded on the polygraph.

Heart Period Change (10 mil. sec.). = .039 inch.

Finger Pulse Amplitude Change (.01% total range) = .00294 inch.

Finger Potential Change (.01 MV) = .00067 inch.

Integrated Muscle Potential Change (.01 μ V) = .0002 inch.

Smoothed GSR (.01 μ mhos) = .00488 inch.

Table 13